

DOCUMENT RESUME

ED 076 900

CG 007 962

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TITLE A Comparison of Brain Wave Patterns of High and Low Grade Point Average Students During Rest, Problem Solving, and Stress Situations.
PUB DATE 73
NOTE 89p.; Doctoral dissertation, University of Maryland
EDRS PRICE MF-\$0.65 HC-\$3.29
DESCRIPTORS Analog Computers; Anxiety; *College Students; Digital Computers; Doctoral Theses; *Electroencephalography; *Grade Point Average; High Achievers; Low Achievers; *Problem Solving; Scientific Research; *Situational Tests; Statistical Analysis; Student Characteristics; Student Research
IDENTIFIERS Brain Wave Patterns

ABSTRACT

The purpose of this study was to compare brain wave patterns produced by high and low grade point average students, while they were resting, solving problems, and subjected to stress situations. The study involved senior midshipmen at the United States Naval Academy. The high group was comprised of those whose cumulative grade point average was between 3.50 and 4.00. The low group was comprised of those whose grade point cumulative average was between 2.00 and 2.25. Instrumentation included a Grass model 79C electroencephalograph, analog/digital filters, digital clocks, digital counters, and an eight channel oscilloscope. Treatment means were evaluated using a repeated measures design and a simple analysis of variance. The following conclusions were reached: (1) There were differences in brain wave patterns, depending whether the subjects were resting, solving problems, or under stress; and (2) The data did not support the hypothesis that high and low grade point average students would have differing brain wave patterns. Several suggestions are made as to areas for future research, and implications of the study are discussed. (Author/LAA)

ED 076900

A COMPARISON OF BRAIN WAVE PATTERNS
OF HIGH AND LOW GRADE POINT AVERAGE STUDENTS
DURING REST, PROBLEM SOLVING, AND STRESS SITUATIONS

by
Karel Montor

Dissertation submitted to the Faculty of the Graduate School
of the University of Maryland in partial fulfillment
of the requirements for the degree of
Doctor of Philosophy
1973

U.S. DEPARTMENT OF HEALTH,
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ACKNOWLEDGMENT

To Dr. Kenneth Hovet, my advisor until his death, I owe a special debt for his long hours of discussion and guidance. It was he who originally helped to make my program of study and who provided that gentle guidance and counsel that enabled me to maximize my study efforts.

The writer also is indebted to his doctoral committee members who raised significant questions during the original design phase and thus stimulated the development of this project. Dr. James Dudley, Chairman, and committee members Dr. John Chapin, Dr. Charles Johnson, Dr. Frank Milhollan, and Dr. Desmond Wedberg supervised the study.

To officers and civilians at the United States Naval Academy, thanks is given for the material and spiritual help provided over the years of my doctoral studies. I am indebted to my family who supported the doctoral efforts over so many years.

Computer time was made available through the facilities of the Computer Science Centers at College Park and Annapolis. The instrumentation was furnished by the United States Naval Academy Research Council and the EEG Laboratory at the Bethesda Naval Hospital.

The voluntary participation by midshipmen of the Class of 1972 is gratefully acknowledged.

TABLE OF CONTENTS

ACKNOWLEDGMENTS ii

LIST OF TABLES v

LIST OF FIGURES vii

Chapter

I. INTRODUCTION 1

 Significance of Problem 1

 Hypotheses to be Researched 2

 Assumptions 3

 Limitations 3

 Procedures 4

 Definitions 5

 Organization of Study 6

II. RELATED RESEARCH 7

 Development of Brain Wave Measurement 7

 EEG Recording Techniques 9

 Relating Brain Waves to Human Behavior 10

 Summary 18

III. METHODS AND PROCEDURES 19

 Design of the Experiment 19

 Description of Subjects 20

 Instrumentation 21

 Testing Procedures 24

 Application of Treatments 25

 Recording of Data 27

 Summary 28

IV.	PRESENTATION AND ANALYSIS OF FINDINGS	29
	Data Related to Theta Brain Wave Measurements	30
	Data Related to Alpha Brain Wave Measurements	35
	Data Related to Beta Brain Wave Measurements	39
	Data Related to Sub-level Brain Wave Measurements	43
	Summary of Findings	47
V.	SUMMARY AND SUGGESTIONS FOR FUTURE RESEARCH	49
	Summary of Study	49
	Findings	50
	Conclusions and Implications	51
	Suggestions for Future Research	52
APPENDIX A.	Data Collection Sheet	55
APPENDIX B.	Raw Scores for Test Nos. 1 through 76	58
APPENDIX C.	ANOVA for Test Nos. 1 through 76	73
SELECTED BIBLIOGRAPHY	77

LIST OF TABLES

Table	Page
I. Differences between High and Low Groups	20
II. Theta Time Mean Scores	31
III. Theta Time Scheffe' Analysis	32
IV. Theta Time Repeated Measures Analysis	33
V. Theta Count Mean Scores	33
VI. Theta Count Scheffe' Analysis	34
VII. Theta Count Repeated Measures Analysis	35
VIII. Alpha Time Mean Scores	35
IX. Alpha Time Scheffe' Analysis	36
X. Alpha Time Repeated Measures Analysis	37
XI. Alpha Count Mean Scores	37
XII. Alpha Count Scheffe' Analysis	38
XIII. Alpha Count Repeated Measures Analysis	39
XIV. Beta Time Mean Scores	39
XV. Beta Time Scheffe' Analysis	40
XVI. Beta Time Repeated Measures Analysis	41
XVII. Beta Count Mean Scores	41
XVIII. Beta Count Scheffe' Analysis	42
XIX. Beta Count Repeated Measures Analysis	43
XX. Sub-level Time Mean Scores	44
XXI. Sub-level Time Scheffe' Analysis	44
XXII. Sub-level Time Repeated Measures Analysis	45
XXIII. Sub-level Count Mean Scores	46

XXIV.	Sub-level Count Scheffe Analysis	46
XXV.	Sub-level Count Repeated Measures Analysis	47

LIST OF FIGURES

Figure	Page
1. Equipment Configuration	22
2. Conceptualization Equipment	26

CHAPTER I

INTRODUCTION

This study had two purposes. The first was to determine if brain wave production differed when college students shifted their attention from (a) resting with their eyes closed, to (b) solving of numerical and conceptual problems, to (c) being faced with stress producing situations and whether these differences were statistically significant. The second purpose was to determine whether high grade point average students produced statistically significant differences in their brain waves while resting, problem solving, and under stress, when compared to low grade point average students.

The subjects were senior midshipmen at the United States Naval Academy. The high group was comprised of those whose cumulative grade point average for their first three years at the Academy was between 3.50 and 4.00. The low group consisted of those whose cumulative grade point average for their first three years at the Academy was between 2.00 and 2.25.

SIGNIFICANCE OF PROBLEM

Through extensive research, development, and modification, educators and psychologists have been able to develop a variety of test instruments which are capable of measuring differences between high and low grade point average students. Ertl, in commenting on the sometimes invalid use of IQ tests, however, has suggested that the

potential for misinterpretation of brain wave analyzed data would be less than with existing pencil and paper tests. The present study is an attempt to add to our knowledge of differences in brain wave production which can be related to differences in academic achievement. The basis of this assumption is that cellular neurological differences may be a contributor rather than a determiner of academic differences.

HYPOTHESES TO BE RESEARCHED

The first research hypothesis was that differing treatments (resting, solving problems, or under stress) would produce significantly different brain waves for all subjects. A sub-hypothesis was that differing treatments produce significantly different theta, alpha, and beta brain wave patterns for all subjects.

The second research hypothesis was that identical treatments applied to students who had high and low grade point averages would result in the production of statistically significant differences in their brain wave patterns. A sub-hypothesis was that students of high grade point average produce significantly different theta, alpha, and beta brain waves than do students of low grade point average.

The differences measured were to be related to the time in seconds that a particular brain wave (theta or alpha or beta) reached or exceeded a 10 microvolt level during a particular treatment. The differences measured were also to be related to the number of times that a

1

William Tracy, "Goodbye IQ, Hello EI (Ertl Index)," Phi Delta Kappan, LIV (October, 1972), 89-94.

particular brain wave reached or exceeded a 10 microvolt level during a particular treatment.

ASSUMPTIONS

The researcher accepted certain basic assumptions regarding the nature and measurement of brain wave patterns in the development and carrying out of this study:

(1) that measurements should be taken between scalp locations O1 and T3 with reference to the International Electrode Placement System (the two points respectively near the back of the head and above the ear);

(2) that measurements should be taken only when brain wave production is at or above 10 microvolts for each of the three frequency bands considered in this study, that is theta, alpha, and beta;

(3) that frequency bands of 4 to 8 Hz (theta), 8 to 13 Hz (alpha), and 13 to 30 Hz (beta) were appropriate for the study.

LIMITATIONS

The findings apply only to the particular groups studied, and generalization to all midshipmen at the United States Naval Academy and/or the general population would be premature until further verifying studies have been completed.

A single resting period and three problem solving treatments were used, each of three minutes duration. However, because two stress treatments were applied, each of one minute duration, the data recorded

during these treatments were increased by a multiple of three so that equivalent data for each treatment could be compared.

The research design did not provide for varying the sequence of treatment application. The decision not to counterbalance was made to insure uniformity of treatment application and subject safety.

PROCEDURES

After the parameters and approaches of the study were determined, specifications were established for equipment configuration. The analog/digital filtering and recording system was specifically built for this study, and the latest solid state electroencephalograph was procured.

Simultaneously with the establishment of the laboratory necessary to conduct this study volunteers were obtained and tested for electroencephalographic normalcy at the Bethesda Naval Hospital. Following application of treatments to all subjects, the data was analyzed on computers at the University of Maryland and the U. S. Naval Academy.

In order that the conclusions be logically and validly applied to the data obtained, care was taken in the design of this study to consider factors relating to internal and external validity.² The following procedural steps were employed:

(1) All treatments were applied within a seventeen minute time frame and the subjects were not told the results of any treatment until

2

Donald T. Campbell and Julian C. Stanley, Handbook of Research on Teaching, ed. N. L. Gage (Chicago: Rand McNally, 1963), p. 171-246.

after all subject testing had been completed.

(2) Equipment was re-calibrated between measurements on each subject.

DEFINITIONS

To provide the reader with the researcher's frame of reference the standard terms and definitions used are presented below:

Treatments -- The recording of brain wave production measurements while the subject rests, solves algebraic problems, solves a three dimensional conceptual problem, does cumulative number adding, and is subjected to two kinds of stress-producing stimuli.

EEG or Electroencephalograph -- A high gain amplifier capable of translating electrical signals produced by the brain into graphic representations. (The EEG used was modified by the addition of analog and digital filtering circuits so that the brain waves produced by the subjects could be converted into discrete digital form.)

Theta Wave -- Those brain wave frequencies between 4 and 8 Hz (cycles per second).

Alpha Wave -- Those brain wave frequencies between 8 and 13 Hz.

Beta Wave -- Those brain wave frequencies between 13 and 30 Hz.

Muscle Artifacts -- Voltages resulting from muscular activity.

Sub-level -- A condition when none of the three brain waves produced by the subject were at or above the 10 microvolt level. (A fourth clock and separate counter tabulated the duration and extent of this state.)

ORGANIZATION OF STUDY

Chapter I provides the basic introduction to the study along with a discussion of the significance of the problem studied and a statement of the hypotheses to be researched. Included are presentations of the assumptions and limitations of the study as well as the procedures and definitions employed.

Chapter II deals with the development of brain wave measurements and brain wave analysis in educational research.

Chapter III concerns itself with the methods and procedures used, including the design of the experiment. The subjects are described along with the design of the instrumentation and testing procedures. The manner of application of treatments and the recording of data are also included in this chapter.

Chapter IV presents and analyzes the findings with respect to the three brain wave areas.

Chapter V summarizes the results of the study and suggests areas for future research.

CHAPTER II

RELATED RESEARCH

This chapter traces the development of brain wave measurement from its inception to the present. The history of relating brain waves to human behavior is less than fifty years old, and this chapter presents some of the findings of researchers who have been trying to relate neurological findings to observed behavior.

DEVELOPMENT OF BRAIN WAVE MEASUREMENT

The technique of measuring brain wave production dates back to the Nineteenth Century. "The first observations on electric potentials of the brain were reported in 1875 by Caton, who with nonpolarizable electrodes and a sensitive galvanometer, recorded currents from the exposed brains of monkeys and rabbits and described the variations of these currents with sleep and approaching death."³ Strauss, Ostow, and Greenstein in tracing the history of the development of brain wave measuring techniques note that "Beck, in 1890, with a galvanometer, first found continuous and spontaneous changes in cerebral potentials not due to any stimulation and independent of the respiratory and

3

H. Strauss, M. Ostow, and L. Greenstein, Diagnostic Electroencephalography (New York. Grune & Stratton, 1952), p. 1.

cardiac rhythms."⁴ On July 6, 1924, Berger made the first recording of a human electroencephalogram.⁵ In 1942 Cohn employed an optomechanical instrument, the cycloscope, to study intracerebral wave patterns.⁶ By 1947 Sonneman and Kennard had reported that they had been able to study by EEG analysis the temporal variability among simultaneously occurring events in the brain.⁷ One of the first steps that was to lead to automatic brain wave analysis was the development in 1948 by Goodwin and Stein of a brain wave correlator which transformed the conventional EEG into square wave patterns independent of the wave form or amplitude from different brain areas.⁸

In 1949 Cohn found that frequency regulation may fluctuate two and one-half hertz per second and still be within the normal range of variation,⁹ while Lilly developed methods offering the possibility for both short time evaluation as well as long term averaging using display systems. These display systems "permit one to observe patterns of illumination by an array of lights over an area, corresponding to the

4

ibid, p. 1.

5

ibid, p. 2.

6

Robert Cohn, "A Cycloscopic Study of the Human Electroencephalogram," Journal of General Physiology, 25 (March, 1942), 517-522.

7

H. Sonneman and M. A. Kennard, "An Interphase Analyzer of the Electroencephalogram," Science, 105 (April, 1947), 437-438.

8

C. W. Goodwin and S. N. Stein, "A Brain Wave Correlator," Science, 108 (November, 1948), 507.

9

Robert Cohn, Clinical Electroencephalography (New York: McGraw-Hill Book Company, 1949), p. 20.

movement of spreading peak voltages over a region of cortex."¹⁰ Burch, in 1959, developed the forerunner of the brain wave measurement technique used in this study. This technique, known as "period analysis," views the EEG data in terms of time intervals between either base-line crossings or successive wave peaks.¹¹ By 1965 Darrow and Hicks illustrated the effect a small attention-getting alerting stimulus has on the EEG.¹² As of this writing, research in brain wave measurement is being aided by the use of on-line computers.¹³

EEG RECORDING TECHNIQUES

Milnarich points out that to record brain waves correctly it is necessary to maintain low electrical resistance between the scalp and electrodes, in order to provide a clear pathway from the brain to the recording instrument.¹⁴ Milnarich also notes that recording artifacts

10

J. C. Lilly, "A Method of Recording the Moving Electrical Potential Gradient in the Brain: A 25-Channel Potential Field Recorder," in Proceedings Second Annual Joint IRE-AIEE Conference on Electronic Instrumentation in Nucleonics and Medicine (New York, 1949), p. 37.

11

N. R. Burch, "Automatic Analysis of the Electroencephalogram: A Review and Classification of Systems," Electroencephalography and Clinical Neurophysiology, 11 (November, 1959), 827-834.

12

C. W. Darrow and R. Hicks, "Interarea EEG Phase Relationships Following Sensory and Ideational Stimuli," Psychophysiology, 1 (April, 1965), 337-346.

13

Peter J. Lang, "The On-Line Computer in Behavior Therapy Research," American Psychologist, 24 (March, 1969), 236-239.

14

Rhoda Feinstein Milnarich, A Manual for EEG Technicians (Boston: Little, Brown and Company, 1958), p. 63.

may interfere with brain wave analysis, and identifies these artifacts as potentials which are recorded on the electroencephalogram but are derived from a source outside the brain. In addition to poor electrode contact, other sources of artifacts, are (1) nonsymmetrical electrode placement, (2) outside electrical interference, (3) defects in apparatus, (4) physiologic potentials arising from sources other than the brain, and (5) uncooperative patients.¹⁵

Strauss, Ostow, and Greenstein stress the importance of the subject being relaxed and they note that "apprehensiveness, emotional stress or excitement sharply depress the amount of alpha activity which is usually replaced by low voltage random frequency activity or by fairly distinct fast activity."¹⁶ Milnarich also points out that "without the cooperation of the patient, an artifact-free record cannot be obtained."¹⁷

RELATING BRAIN WAVES TO HUMAN BEHAVIOR

This section will review efforts of selected researchers to establish a relationship between brain waves and human behavior. In 1940 Knott found that the primary difficulty in relating brain waves to human behavior had to do with (1) records not being taken under conditions involving intellectual behavior, and (2) that while alpha

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ibid, p. 69.

16

op.cit., p. 25.

17

op.cit., p. 42

activity can be looked at fairly carefully, that wasn't true of the entire EEG record.¹⁸

While progress has been made over the years in relating EEG recordings to human behavior, the analysis of brain waves has not been without disagreement respecting the significance of the research findings. The remainder of this section will place in chronological perspective the doubts as well as the accomplishments claimed.

EEG record analysis had only been in existence a mere fifteen years when Lindsley, in 1944, indicated that there was little chance that a high degree of relationships would be found between EEG recordings and intelligence.¹⁹ Nosal, reporting on the research of Schwab, noted that as of 1950 it had been found that increments in slow wave activity were present during periods of mental effort.²⁰ Contradictory interpretations of results achieved are pointed out by Nosal relative to the work of Ostow who maintained that, as of 1950, a relationship had not yet been found between EEG records and intelligence.²¹

In 1952, on the other hand, MacKay and McCulloch theorized that

18

John R. Knott, "The Physiological Correlates of Intelligence," in NSSE Thirty-Ninth Yearbook, Part 1: Intelligence: Its Nature and Nurture (Bloomington: Public School Publishers, 1940), Chapter 4.

19

D. B. Lindsley, "Electroencephalography," in Personality and Behavior Disorders, ed. J. McV. Hunt (New York: Ronald Press, 1944), pp. 1033-1103.

20

Walter S. Nosal, A Primer for Counseling the College Male (Dubuque: Wm. C. Brown Book Company, 1968), p. 133.

21

ibid, p. 310.

information is transmitted as a spike interval code.²² (As previously reported on page nine of this chapter, in 1959 Burch developed a means of measuring these spikes.)

A 1956 analysis by Ellingson indicated his belief that little had been accomplished with respect to finding correlations between EEG records and intelligence since the 1944 Lindsley review.²³ Yet a year later (1957), Mundy-Castle completed a study which indicates that new knowledge in the field was being gained:

Our first finding was confirmation of the hypothesis that alpha frequency would be significantly correlated with Vocabulary. It was also significantly correlated with Verbal IQ, Practical IQ, and General IQ. The relevant conclusion for the present context is that the amount of alpha rhythm present in an EEG is in part related to the extent to which visual imagery is used during thought, and that persons who think predominately in visual images tend to possess "minus" type (low voltage, low index) alpha rhythms, whereas those who think predominately by verbal-motor imagery tend to possess "persistent" (medium to high voltage, high index) alpha rhythms.²⁴

A major analysis of past research, by Vogel and Broverman in 1964, of the relationship between EEG and test intelligence concluded that (1) "the bulk of the studies with feebleminded subjects, children, institutionalized geriatric subjects, and brain-injured adults have reported a significant EEG-test intelligence relationship," and (2)

22

D. M. MacKay and W. S. McCulloch, "The Limiting Information Capacity of a Neuronal Link," Bulletin of Mathematical Biophysics, 14 (June, 1952), 127-135.

23

R. J. Ellingson, "Brain Waves and Problems in Psychology," Psychological Bulletin, 53 (January, 1956), 1-34.

24

From Nosal, op.cit., p. 131.

"investigators who have studied normal adults have not found significant relationships between test intelligence and EEG tracings;" however, (3) "in every case in which test intelligence has been found to be related to EEG frequencies, low intelligence was associated with slow alpha frequencies and the presence of the slower EEG rhythms (delta and theta). Conversely, higher levels of intelligence were found associated with the fast alpha frequencies and an absence of the slow delta and theta rhythms."²⁵

Ellingson in his 1966 review of the Vogel and Broverman report agreed that "the weight of available evidence suggests that there is no relationship in normal adults"²⁶ between brain waves and intelligence. Ellingson did, however, disagree with another of their conclusions and he stated his belief that "the evidence concerning relationships between normal brainwave phenomena and intelligence in children and in the mentally retarded is contradictory and inconclusive."²⁷

Ellingson further "confesses to a continuing pessimism about finding significant and important relationships between EEG phenomena and complex behavioral processes."²⁸ He further indicates that "if

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William Vogel and Donald M. Broverman, "Relationship Between EEG and Test Intelligence: A Critical Review," Psychological Bulletin, 62 (August, 1964), 132-144.

26

Robert J. Ellingson, "Relationship Between EEG and Test Intelligence: A Commentary," Psychological Bulletin, 65 (February, 1966), 96.

27

ibid, p. 96.

28

ibid, p. 96.

relationships between complex behavior and brain electrical activity are to be found it is more likely that they will be found by recording brain electrical activity during S-R sequences, than during rest and relaxation."²⁹ On their part Vogel and Broverman, commenting on Ellingson's review of their 1964 paper, conclude that Ellingson's commentary is based essentially upon mistakes of fact and faulty assessment of the data.³⁰

In 1965, Sutton, Braren, Zubin, and John reported that "components of the AEP (average evoked potential) are most sensitive to changes in stimulus parameters involving decision making."³¹ (This supports the theory reported on page eleven of this chapter, by MacKay and McCulloch, that "information is transmitted as a spike interval code.") The 1967 findings of Roy, Herrington, and Sutton "suggest that the waveform of evoked responses is not determined solely by the set of peripheral receptors which is stimulated but it also reflects the perceptual content of the stimulus."³²

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ibid, p. 96.

30

William Vogel and Donald M. Broverman, "A Reply to "Relationship Between EEG and Test Intelligence: A Commentary," Psychological Bulletin, 65 (February, 1966), 99.

31

S. Sutton, M. Braren, J. Zubin, and E. R. John, "Evoked Potential Correlates of Stimulus Uncertainty," Science, 150 (November, 1965), 1187-1188.

32

E. Roy, R. N. Herrington, and Samuel Sutton, "Effects of Visual Form on the Evoked Response," Science, 155 (March, 1967), 1439.

From the mid-1960's to this time, the preponderance of evidence suggests that correlated relationships have been found between EEG records and human behavior. One exception to this, is a report by Nosal in 1968 in which he reports finding no significant differences between college student "leaders" and "underachievers" with respect to their alpha production.³³ Since the finding did not fully parallel the results of this study, Dr. Nosal was contacted by phone during October 1972 and the procedures used during the two studies were compared. The essential methodological difference had to do with the measurement of alpha production in the Nosal study being by "eye," while the measurements taken in this study were generated by analog/digital filter analysis. An "eye" analysis of the EEG records in this study by an experienced neurologist also failed to establish the significant differences which can, in fact, be found by analog/digital filter analysis as was done in this research.

In 1968 Bennett reported that a correlation coefficient of .593 was found between the Wechsler adult intelligence scale and the dominant brain wave frequency of the individual, with dominant frequency increasing with IQ. He did note that "a correlation of unity with an IQ test could not be expected for this type of test, as the IQ test is intended to measure all aspects of intelligence, including memory and environmental effects, whereas this work measures only the electrical

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op.cit., p. 175.

characteristics of the visual pathway."³⁴

Pribram has observed that "changes in EEG frequency relate more to the balance between cellular synchrony and desynchrony than to the specific information content of a signal. If recorded with adequate resolution, they may indicate where the action is, but not what the action is all about."³⁵ Pribram further comments that "the most reliable sign of active neuronal processing of sensory information is differentiation and diversification of cellular firing patterns, as expressed by desynchronization of the EEG."³⁶ Confirming the findings of Sutton, Braren, Zubin, and John discussed on page fourteen of this chapter Pribram observes that "in continued problem solving behavior, increasingly complex patterns of neural events occur."³⁷

Ertl has found correlations ranging from 0.30 to 0.50 between IQ test scores and parameters of the visual evoked potential which he reports in a 1969 study with a sample of 300 children whose mean age was 124 months with a range from 86 to 185 months.³⁸ In regard to these

34

W. F. Bennett, "Human Perception: a Network Theory Approach," Nature, 220 (December, 1968), 1148.

35

K. H. Pribram, Brain and Behaviour 2 - Perception and Action (Baltimore: Penguin Books Inc., 1969), p. 63.

36

ibid, p. 62

37

K. H. Pribram, Brain and Behaviour 4 - Adaptation (Baltimore: Penguin Books Inc., 1969), p. 167.

38

J. P. Ertl, "Evoked Potentials, Neural Efficiency, and IQ," in Biocybernetics of the Central Nervous System, ed. Lorne D. Proctor (Boston: Little, Brown and Company, 1969), p. 427.

findings, the words of Mundy-Castle in a 1958 article seem appropriate. He points to the importance of using correct statistical procedures and observes, with respect to past studies where differences in results were found with reference to psychological correlates of EEG variability, that these differences may well have been partially due to sampling influences.³⁹

In 1969 Ertl reported that "the AEP's of the high IQ subjects are more complex, characterized by high frequency components in the first 100 milliseconds which are not observed in the AEP's of the low IQ subjects. The ten high IQ subjects had a mean E3 (third sequential peak) latency of eighty-eight milliseconds while the low IQ subjects had a mean E3 latency of 194 milliseconds."⁴⁰

In 1971 Ertl indicated the complexity of brain wave analysis he felt would be necessary to achieve meaningful results:

Components of the AEP correspond to neural events in the processing of information in the brain; the latency of these components is very stable but their amplitude and spectral characteristics are not. Any analysis which depends on average characteristics of the AEP over an interval of time may be hard to relate to human intelligence. Analyses which are based on ratios, relative to component amplitudes, peak latencies, the first and second derivatives of the AEP, and so forth, seem more promising.⁴¹

39

A. C. Mundy-Castle, "Electrophysiological Correlates of Intelligence," Journal of Personality, 26 (March, 1958), 184-199.

40

John P. Ertl and Edward W. P. Schafer, "Brain Response Correlates of Psychometric Intelligence," Nature, 223 (July, 1969), 422.

41

John P. Ertl, "Fourier Analysis of Evoked Potentials and Human Intelligence," Nature, 230 (April, 1971), 526.

SUMMARY

This chapter has reviewed the history of the development of brain wave measurements from its inception to the present use of computers, as well as the efforts to relate brain wave measurements to human behavior. Although the literature search conducted as part of this study did not find reports relating EEG data to achievement, it is known that such studies are being planned by the Langley Porter Neuropsychiatric Research Institute. Though it is evident at this writing that researchers have decades and centuries of work ahead of them, enough has been learned already to justify further efforts.

We do know how to detect the existence of electrochemical activity in the brain as well as how to classify and recognize some of its more gross components. Scientific advances in wave analysis in general have allowed application of known theory to brain wave measurement to the point that today, using a super-cooled magnetometer in a shielded environment, it is possible to detect brain wave activity without electrical contact with the scalp.

A continuing limiting factor with respect to research in this area will be the cost of equipment required to do brain wave measurement. Another hindrance is the extended periods of time required to perform both the tests and subsequent evaluations of data acquired. Despite the limitations, the increasing effort in the field of brain wave research suggests that progress in the future will be swifter than it has been in the past.

CHAPTER III

METHODS AND PROCEDURES

This experiment was designed to test the hypotheses that: (1) brain wave patterns would be different, depending whether the subjects were resting, solving problems, or under stress; and (2) that high and low grade point average students would have differing brain wave patterns. The experiment required (1) the identification of students to be evaluated, (2) the development of instruments to measure the data to be analyzed, (3) the establishment of testing procedures, (4) the determination of the form that treatments should take, and (5) the recording and analysis of data.

This chapter describes the general design of the experiment, contains a description of the procedures followed in accomplishing the tasks enumerated above, includes a description of the subjects used in the experiment, and describes the gathering of the data and the procedures used in analyzing the data.

DESIGN OF THE EXPERIMENT

After establishing the basic research hypotheses, it was determined that objective measurements and analyses would be facilitated by insuring that all data to be observed and analyzed were of digital form. The next step was to determine what types of treatments could lead to the generation of data suitable for hypotheses testing.

After treatments were determined, equipment was designed and

procured that had as its end product easily read digital results. A neurologist evaluated volunteer subjects for neurological normalcy, and treatment application was performed during November, 1971. The final step was the computer analysis of brain wave generated data in accordance with the treatment by Winer as described in his "Multifactor Experiments Having Repeated Measures on the same Element."⁴²

DESCRIPTION OF SUBJECTS

All senior midshipmen at the United States Naval Academy whose grade point average for the first three years was either between 3.50 and 4.00 or between 2.00 and 2.25 were identified. Further differences between the two groups are presented below in Table 1 (extracted from Appendix C).

Table I
DIFFERENCES BETWEEN HIGH AND LOW GROUPS

College Board Examination Area	Mean		Std. Dev.		F	
	High	Low	High	Low		
Aptitude-Verbal	634.3	566.5	75.4	48.0	13.8	p < .01
Aptitude-Math	697.6	633.3	47.4	67.4	14.6	p < .01
Achievement- English Comp.	611.1	556.5	72.7	61.0	7.9	p < .01
Achievement-Math	727.2	620.0	58.0	54.9	43.3	p < .01
Rank in HS Class	650.0	508.1	96.4	78.2	31.4	p < .01

42

B. J. Winer, Statistical Principles in Experimental Design
(New York: McGraw-Hill Book Company, 1962), Chapter 7, pp. 298-312.

In accordance with standard procedures efforts were made to secure volunteers without undue pressure exerted on them to participate. Of the fifty-four men identified in the high group, twenty-eight volunteered, and twenty-five of these were determined to be free of muscle artifacts. Of the 149 men identified in the low group, twenty-nine were accepted as volunteers and twenty-five of these were determined to be free of muscle artifacts.

All testing was accomplished during the evening hours in an attempt to reduce the differences in EEG rhythms that would be due solely to the testing of individuals at various times during the twenty-four hour day.⁴³ All data from these tests appear in Appendix B:

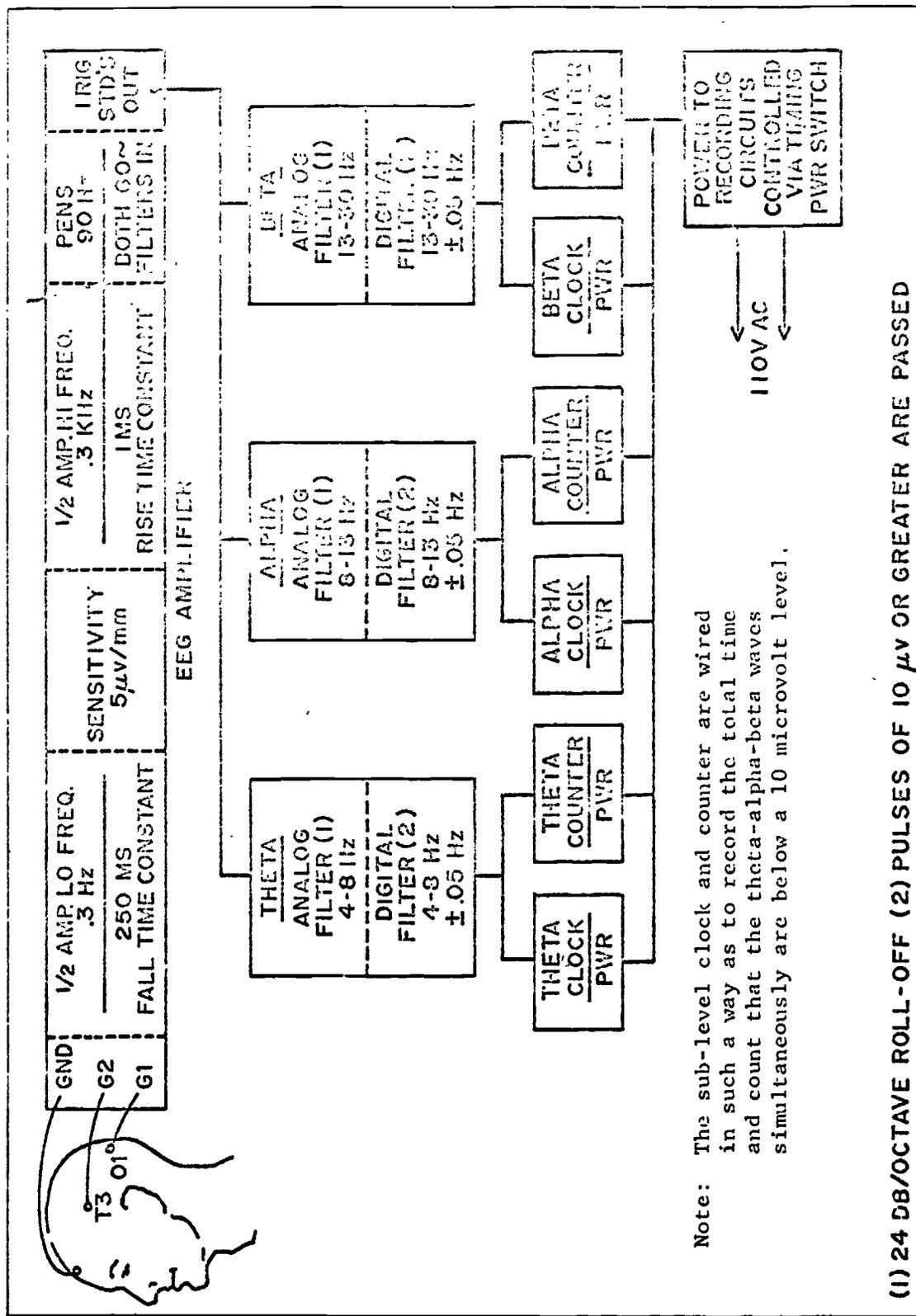
INSTRUMENTATION

The entire instrumentation, with the exception of the sub-level circuitry, is graphically presented in Figure No. 1 on page 22.

The following frequency ranges were established in measuring the dependent variable. Recording was limited to brain wave production at or greater than 10 microvolts: theta 4 to 8 Hz, alpha 8 to 13 Hz, and beta 13 to 30 Hz. The EEG measurements were taken from O1 to T3, based on the International Electrode Placement System. Filters were used to measure simultaneously all three theta-alpha-beta brain wave states. Inter-electrode resistance between O1 and T3 was below 10,000 ohms for all subjects to avoid contamination from spurious artifacts.

43

Gay Gaer Luce, Biological Rhythms in Human and Animal Physiology (New York: Dover Publications, 1971), p. 57.



Note: The sub-level clock and counter are wired in such a way as to record the total time and count that the theta-alpha-beta waves simultaneously are below a 10 microvolt level.

(1) 24 DB/OCTAVE ROLL-OFF (2) PULSES OF 10 μV OR GREATER ARE PASSED

Fig. 1 Equipment Configuration

One channel of a model 79C Grass electroencephalograph was used to pick up the brain wave signals. G1 was attached to O1, G2 was attached to T3, and a ground wire was placed in the middle of the forehead to minimize sixty cycle current effects. The brain wave signals were then fed into a filtering system (see Figure 1) which first used analog filters to establish the general range of theta (4 to 8 Hz), alpha (8 to 13 Hz), and beta (13 to 30 Hz). These signals were next fed into individual digital filters for each channel, so that subsequent outputs were known to lie within limits accurate to plus or minus .05 Hz. The filtering system was adjusted in such a way that only those theta and/or alpha and/or beta brain wave signals at or higher than 10 microvolts (10 uv) would be passed. Thus, all measurements noted in this study should be understood to be with reference to a 10 uv cut-off level, with theta-alpha-beta readings being at or above that level.

When a theta-alpha-beta signal was at or above the 10 uv level a relay closed and upon this action a digital clock recorded the length of this period to within one-hundredth of a second. In parallel with this clock was a counter that recorded the initial closing of the relay. At the end of a treatment it was possible to know and record for each of the three brain wave states how many total seconds the wave had been at or above the 10 uv level, and also how many times the signal went above and below the 10 uv level.

In addition, a fourth recording feature was added and it operated through the relays recording the other three brain wave changes. When

all three waves were simultaneously below the 10 uv level a fourth relay was closed and it in turn operated both a clock and a counter. These are referred to in this report as sub-level readings.

TESTING PROCEDURES

Upon arrival at the brain wave research laboratory each subject had explained to him what directions he was expected to follow. Using procedures recommended by the EEG manufacturer electrodes were attached and inter-electrode resistance checked to insure that impedance was less than 10,000 ohms. The subject was advised that questions they might have during the experiment would be answered at the end of the testing period. The subjects were read all further instructions in order to maintain uniformity.

During treatments all wave forms were monitored on an oscilloscope to detect muscle artifacts should they be present and thus permit invalidating a subjects record. At the end of each treatment applied to each subject, the digital clocks and counters were read and the data recorded. The equipment was then zeroed for the next treatment.

In answer to the question most often asked - "How did I do?" - the subjects were told that this was a group experiment and it was not possible to evaluate the data on any one subject until all data for all subjects had been gathered and analyzed. Each subject was thanked for his participation and, after he left, an equipment calibration check was run to insure that the equipment was still in calibration and ready for the next subject.

The actual treatments were fourteen minutes in length and the total time from start of the first treatment to completion of the last was seventeen minutes. The total time allowed for greeting the subject, hooking him up, application of treatments, questions and answers, and washing him off was fifty minutes. Five additional minutes were scheduled for equipment calibration, and five minutes provided for the researcher to rest prior to the next subject's arrival.

APPLICATION OF TREATMENTS

Resting. Subjects were seated in a reclining chair and asked to remain quiet, with their eyes closed. Treatment length was three minutes.

Mathematics Problem. The subject was disconnected from the EEG and then shifted from the reclining chair to a desk-chair and then re-connected to the EEG. Problems presented to the subject for solution follow:

1. If a car leaves Annapolis at 1545 heading for New York City at an average rate of 57 miles per hour, how far from its destination will it meet a car that left New York City the same day at 1515 that is heading for Annapolis at an average rate of 43 miles per hour. Assume that the distance between the two cities is 287 miles.
2. If it takes 987 men 1435 days to build an aircraft carrier-how long will it take to build the same carrier if we are able to replace the slowest 17% of the men with workers who can accomplish twice as much per unit hour worked. Assume 253 working days per year and $8\frac{1}{2}$ hours per working day.
3. A ship leaves Baltimore harbor at 0350 heading for San Diego-how far will it have gone after 242 hours assuming that it goes around the tip of South America and starts out at an average speed of 23 knots and increases that by 6% per day.

Treatment length was three minutes.

Conceptual Problem. The subject remained on the desk-chair. The working papers and writing instrument used in conjunction with the previous treatment were taken away and in their place was substituted the pyramid puzzle illustrated in Figure 2 below.

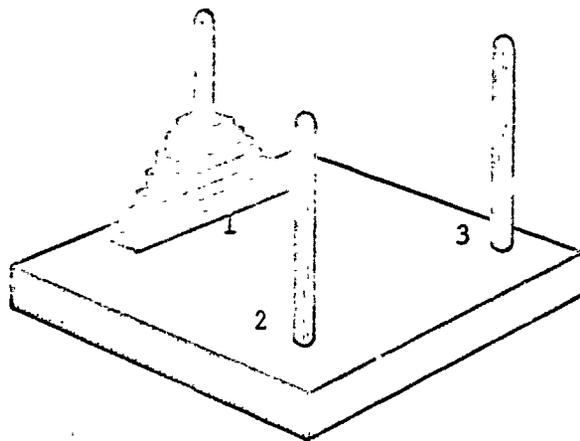


Fig. 2 Conceptualization Equipment

Subjects were instructed to try and accomplish the transfer of the pile of pieces from the number 1 peg to either of the other without moving more than one piece at a time and never putting a larger piece on a smaller one. They were advised that they could move the pieces back and forth on all three pegs as often as they wanted. The objective was to re-build the pyramid on either the number 2 or number 3 peg. Treatment length was three minutes.

Cumulative Number Adding Problem. The subject remained at the desk-chair. Instructions were given to the subject to add in his mind, "without announcing the results, 1 plus 2 which gives 3." His next

operation was to "then add 3 to this total giving 6; then add 4 to that total giving 10; then add 5 to that total giving 15, and so on until told to stop." Treatment length was three minutes.

Color Stress. The subject remained at the desk-chair, and was shown a card on which were printed the names of various colors. The ink used to print each word was in a different color than that spelled by the letters of the word. For example, blue was written in green ink. The subject was asked to say out loud the color of the ink in which each word was printed. Treatment length was one minute.

Syringe Stress. The subject remained at the desk-chair. During the one minute duration of this treatment, the researcher (1) tied a restrictor around the arm of the subject, (2) cleared the air from a syringe, (3) cleaned the arm with alcohol, and (4) brought the syringe up to the subject's arm. The one minute period ended when the needle was approximately a half a centimeter away from the subject's skin.

At this point the subject was told that the experiment was over for him and that he could ask questions. Electrodes were removed after all questions had been answered.

RECORDING OF DATA

At the end of each treatment, the digital data appearing on the clocks and counters were recorded on prepared data sheets. Key punching of data was done after all subjects had been tested. Simple ANOVA analyses were performed on the computer at the United States Naval Academy. A repeated measures design was run by the Computer Science

Center at the University of Maryland in the spring of 1972.

SUMMARY

This chapter has reviewed the general design of the experiment from (1) the initial decision to procure equipment which would have easily read digital clocks and counters, through (2) determination of treatments to be used, to (3) the selection of subjects. Also included is the instrumentation configuration, testing procedures, application of treatments to subjects, and the recording of data.

Because electrical and mechanical interface characteristics were thoroughly developed before any equipment was ordered or built, the construction and assembly of the brain wave research laboratory was accomplished without significant difficulty.

The pre-evaluation of subjects for muscle artifacts proved necessary since close to 11% of the volunteers generated signals which would have interfered with the collection of uncontaminated brain wave signals.

The importance of preliminary practice in application of treatments was emphasized so that the results obtained would not be biased by the researcher's shifting procedures from one subject to the next.

Future experimenters would probably benefit by tape recording the brain wave signals for subsequent data reduction, thus permitting a smooth transition from one treatment to the next without the necessity of transcribing the results after each treatment.

CHAPTER IV

PRESENTATION AND ANALYSIS OF FINDINGS

This investigation was designed to test the hypotheses that brain wave patterns would be different, depending whether the subjects were resting, solving problems, or under stress. Collaterally, it was hypothesized that high and low grade point average students would have differing brain wave patterns.

Brain wave measures were obtained for each of fifty subjects, twenty-five proven high achievers and twenty-five established as lower achievers, by administering to each of the subjects at individual times the following treatments in the same sequence.

1. Resting

Problem Solving

2. Mathematical
3. Conceptualization
4. Cumulative Number Adding

Stress

5. Color
6. Syringe

Appropriate F statistics were computed to permit estimation of the statistical significance of the difference between means. A two dimensional repeated measures design with repetition on the A dimension only, following a Lindquist Type I design, was the approach taken for analysis of brain wave measures. This design enabled a comparison of means, both those between high and low achievers as well as among treatment means. The assumption of homogeneity of covariance was tested

and supported. The assumption of homogeneity of equicovariance was tested and not supported, resulting in an adjustment in the calculation of the F statistic relating variability among the means of the six treatments, and significance of interaction relative to the difference between the variabilities within high and low.

Because the assumption of homogeneity of equicovariance was not supported, a simple analysis of variance was calculated comparing means among subjects for each treatment. Appendix C provides a summary of all simple ANOVA calculations that compared the means of highs against lows for all treatments.

During each treatment, brain wave activity in the three ranges - theta (4 to 8 Hz), alpha (8 to 13 Hz), and beta (13 to 30 Hz) - were recorded when the brain wave signals reached or exceeded 10 microvolts in amplitude. The number of times during each treatment that the brain wave signals were at or above the 10 uv level were recorded on digital counters. The cumulative length of time to the nearest one-hundredth of a second that the brain wave signals were at 10 uv or more during each treatment was also recorded. Appendix A, in association with Appendix B, identifies the time and count data recorded during this study for all three theta-alpha-beta brain wave measurements.

DATA RELATED TO THETA BRAIN WAVE MEASUREMENTS

The theta time mean scores and their associated standard deviations for the six treatments are presented in Table II on page 31. The display of the mean figures to two places and standard deviations to one

in this and subsequent presentations is done to simplify the task of reading the table.

Table II
THETA TIME MEAN SCORES

		<u>Rest-</u> <u>ing</u>	<u>Math</u> <u>Prob</u>	<u>Con-</u> <u>cep-</u> <u>tual</u> <u>Prob</u>	<u>Cum-</u> <u>num</u> <u>Prob</u>	<u>Color</u> <u>Stress</u>	<u>Syringe</u> <u>Stress</u>	<u>Total</u>
High	<u>Mean</u>	<u>103.56</u>	<u>55.98</u>	<u>69.48</u>	<u>52.17</u>	<u>55.35</u>	<u>47.79</u>	<u>64.05</u>
	<u>S.D.</u>	<u>29.5</u>	<u>21.8</u>	<u>17.9</u>	<u>23.6</u>	<u>20.7</u>	<u>19.8</u>	<u>29.5</u>
Low	<u>Mean</u>	<u>87.46</u>	<u>57.86</u>	<u>73.88</u>	<u>56.38</u>	<u>65.31</u>	<u>52.14</u>	<u>65.50</u>
	<u>S.D.</u>	<u>40.6</u>	<u>20.4</u>	<u>19.2</u>	<u>31.1</u>	<u>25.8</u>	<u>21.9</u>	<u>30.1</u>
Total	<u>Mean</u>	<u>95.51</u>	<u>56.92</u>	<u>71.68</u>	<u>54.27</u>	<u>60.33</u>	<u>49.97</u>	
	<u>S.D.</u>	<u>36.8</u>	<u>21.4</u>	<u>18.9</u>	<u>28.0</u>	<u>24.0</u>	<u>21.3</u>	

A Scheffe analysis indicating significance of difference between total treatment mean scores appears in Table III on page 32. Included in this table is a graphic representation of the mean score values.

TABLE IV
THETA TIME REPEATED MEASURES ANALYSIS

Source	DF	SS	MS	F	
Among Subjects					
B	1	159.37	159.37	.07	
Subjects(s)	48	103849.55	2163.53		
Within Subjects					
A	5	70164.69	14032.94	39.22	$p < .05$
AB	5	5063.36	1012.67	2.83	
AS	240	85862.22	357.76		
Total	299	265099.19			

The theta count mean scores and their associated standard deviations for the six treatments are shown in Table V below.

TABLE V
THETA COUNT MEAN SCORES

		<u>Rest- ing</u>	<u>Math Prob</u>	<u>Con- cep- tual Prob</u>	<u>Cum- num Prob</u>	<u>Color Stress</u>	<u>Syringe Stress</u>	<u>Total</u>
High	<u>Mean</u>	<u>211.60</u>	<u>165.00</u>	<u>190.64</u>	<u>153.08</u>	<u>165.72</u>	<u>144.48</u>	<u>171.75</u>
	<u>S.D.</u>	<u>35.2</u>	<u>44.8</u>	<u>23.9</u>	<u>47.6</u>	<u>40.5</u>	<u>50.7</u>	<u>47.4</u>
Low	<u>Mean</u>	<u>185.48</u>	<u>168.36</u>	<u>195.28</u>	<u>156.36</u>	<u>177.84</u>	<u>151.68</u>	<u>172.50</u>
	<u>S.D.</u>	<u>67.6</u>	<u>36.7</u>	<u>25.8</u>	<u>62.2</u>	<u>39.3</u>	<u>46.5</u>	<u>51.1</u>
Total	<u>Mean</u>	<u>198.54</u>	<u>166.68</u>	<u>192.96</u>	<u>154.72</u>	<u>171.80</u>	<u>148.08</u>	
	<u>S.D.</u>	<u>56.0</u>	<u>41.4</u>	<u>25.2</u>	<u>56.0</u>	<u>40.8</u>	<u>49.2</u>	

A Scheffé analysis indicating significance of difference between total treatment mean scores appears in Table VI on page 34. Included in this table is a graphic representation of the mean score values.

TABLE VII
THETA COUNT REPEATED MEASURES ANALYSIS

Source	DF	SS	MS	F	
Among Subjects					
B	1	41.75	41.75	.01	
Subjects(s)	48	336521.75	7010.87		
Within Subjects					
A	5	102135.62	20427.12	17.86	p<.05
AB	5	11515.12	2303.02	2.01	
AS	240	274441.00	1143.50		
Total	299	724655.25			

DATA RELATED TO ALPHA BRAIN WAVE MEASUREMENTS

The alpha time mean scores and their associated standard deviations for the six treatments are presented in Table VIII below.

TABLE VIII
ALPHA TIME MEAN SCORES

		<u>Rest- ing</u>	<u>Math Prob</u>	<u>Con- cep- tual Prob</u>	<u>Cum- num Prob</u>	<u>Color Stress</u>	<u>Syringe Stress</u>	<u>Total</u>
High	<u>Mean</u>	<u>160.20</u>	<u>121.46</u>	<u>127.21</u>	<u>125.50</u>	<u>117.03</u>	<u>113.18</u>	<u>127.43</u>
	<u>S.D.</u>	<u>13.9</u>	<u>17.6</u>	<u>12.1</u>	<u>23.6</u>	<u>21.0</u>	<u>21.0</u>	<u>24.3</u>
Low	<u>Mean</u>	<u>141.32</u>	<u>120.80</u>	<u>124.37</u>	<u>117.55</u>	<u>124.29</u>	<u>113.67</u>	<u>123.67</u>
	<u>S.D.</u>	<u>33.3</u>	<u>20.3</u>	<u>19.4</u>	<u>32.3</u>	<u>20.7</u>	<u>24.9</u>	<u>27.3</u>
Total	<u>Mean</u>	<u>150.76</u>	<u>121.13</u>	<u>125.79</u>	<u>121.53</u>	<u>120.66</u>	<u>113.42</u>	
	<u>S.D.</u>	<u>27.5</u>	<u>19.2</u>	<u>16.4</u>	<u>28.9</u>	<u>21.3</u>	<u>23.3</u>	

A Scheffe analysis indicating significance of difference between total treatment mean scores appears in Table IX below. Included in this table is a graphic representation of the mean score values.

TABLE IX
ALPHA TIME SCHEFFE ANALYSIS

		<u>Treatment</u>	<u>Time(in seconds)</u>
<u>S indicates p<.05</u>		1. Rest	155
1 vs 2,3,4 - S		<u>Problem Solving</u>	150
1 vs 5,6 - S			145
2,3,4 vs 5,6 -		2. Mathematical	140
		3. Conceptualization	135
		4. Cumulative Number Adding	130
	<u>6</u>		125
	<u>5</u>		120
	<u>4</u>	<u>Stress</u>	115
	<u>3</u>		110
<u>2</u>	S	5. Color	
<u>1</u>	S S S S S	6. Syringe	

Treatment	Time (in seconds)
1	155
2	150
3	145
4	140
5	130
6	120

The two dimensional repeated measures analysis for data recorded on the alpha clock appears in Table X on page 37. The Within Subjects F statistic of 31.40 indicates significance at the .05 level with respect to variability among the means of the six treatments. This further supports the hypothesis, with relation to alpha time, that: "Brain wave patterns would be different, depending whether the subjects were resting, solving problems, or under stress."

A simple ANOVA comparing high and low groups for each treatment condition resulted in a significant F statistic for the resting treatment of 6.6 which is significant at the .025 level, and is shown in Appendix C. A simple ANOVA comparing high and low groups for each of

the other five treatment conditions resulted in no significant differences.

TABLE X
ALPHA TIME REPEATED MEASURES ANALYSIS

Source	DF	SS	MS	F	
Among Subjects					
B	1	1068.06	1068.06	.59	
Subjects(s)	48	87520.25	1823.34		
Within Subjects					
A	5	42127.25	8425.45	31.40	p < .05
AB	5	4947.25	989.45	3.69	
AS	240	64400.25	268.33		
Total	299	200063.06			

The alpha count mean scores and their associated standard deviations for the six treatments are shown in Table XI below.

TABLE XI
ALPHA COUNT MEAN SCORES

		<u>Rest- ing</u>	<u>Math Prob</u>	<u>Con- cep- tual Prob</u>	<u>Cum- num Prob</u>	<u>Color Stress</u>	<u>Syringe Stress</u>	<u>Total</u>
High	<u>Mean</u>	<u>120.08</u>	<u>300.60</u>	<u>305.88</u>	<u>255.76</u>	<u>305.40</u>	<u>281.64</u>	<u>261.56</u>
	<u>S.D.</u>	<u>54.7</u>	<u>28.7</u>	<u>22.3</u>	<u>59.7</u>	<u>30.3</u>	<u>33.0</u>	<u>77.4</u>
Low	<u>Mean</u>	<u>176.92</u>	<u>303.28</u>	<u>307.12</u>	<u>263.00</u>	<u>304.44</u>	<u>289.56</u>	<u>274.05</u>
	<u>S.D.</u>	<u>96.4</u>	<u>30.1</u>	<u>28.4</u>	<u>78.8</u>	<u>42.9</u>	<u>41.4</u>	<u>74.9</u>
Total	<u>Mean</u>	<u>148.50</u>	<u>301.94</u>	<u>306.50</u>	<u>259.38</u>	<u>304.92</u>	<u>285.60</u>	
	<u>S.D.</u>	<u>84.2</u>	<u>29.7</u>	<u>25.8</u>	<u>70.7</u>	<u>37.4</u>	<u>38.1</u>	

A Scheffé analysis indicating significance of difference between

total treatment mean scores appears in Table XII below. Included in this table is a graphic representation of the mean score values.

TABLE XII
ALPHA COUNT SCHEFFE ANALYSIS

		<u>Treatment</u>	<u>Relay Closures</u>
<u>S indicates p<.05</u>		1. Rest	320
1 vs 2,3,4	- S	<u>Problem Solving</u>	300
1 vs 5,6	- S		280
2,3,4 vs 5,6	-	2. Mathematical	260
		3. Conceptualization	240
		4. Cumulative Number Adding	220
		<u>Stress</u>	200
			180
			160
			140
		5. Color	
		6. Syringe	

	1	2	3	4	5	6
<u>1</u>	S	S	S	S	S	S
<u>2</u>	S	S	S	S	S	S
<u>3</u>	S	S	S	S	S	S
<u>4</u>	S	S	S	S	S	S
<u>5</u>	S	S	S	S	S	S

The two dimensional repeated measures analysis for data recorded on the alpha counter can be found in Table XIII on page 39. The Within Subjects F statistic of 84.70 indicates significance at the .05 level with respect to variability among the means of the six treatments. This further supports the hypothesis, with relation to alpha count, that: "Brain wave patterns would be different, depending whether the subjects were resting, solving problems, or under stress."

A simple ANOVA comparing high and low groups for each treatment condition resulted in a significant F statistic for the resting treatment of 6.3 which is significant at the .025 level, and is shown in Appendix C. A simple ANOVA comparing high and low groups for each of

the other five treatment conditions resulted in no significant differences.

TABLE XIII
ALPHA COUNT REPEATED MEASURES ANALYSIS

Source	DF	SS	MS	F	
Among Subjects					
B	1	11706.25	11706.25	2.37	
Subjects(s)	48	237217.75	4942.04		
Within Subjects					
A	5	933067.25	186613.45	84.70	p < .05
AB	5	30238.25	6047.65	2.74	
AS	240	528787.50	2203.28		
Total	299	1741017.00			

DATA RELATED TO BETA BRAIN WAVE MEASUREMENTS

The beta time mean scores and their associated standard deviations for the six treatments can be found in Table XIV below.

TABLE XIV
BETA TIME MEAN SCORES

		Rest- ing	Math Prob	Con- cep- tual Prob	Cum- num Prob	Color Stress	Syringe Stress	Total
High	Mean	<u>58.57</u>	<u>117.32</u>	<u>119.26</u>	<u>89.50</u>	<u>115.56</u>	<u>93.87</u>	<u>99.01</u>
	S.D.	21.5	27.9	25.4	34.6	32.7	35.7	37.1
Low	Mean	<u>47.54</u>	<u>119.04</u>	<u>120.01</u>	<u>91.09</u>	<u>132.45</u>	<u>105.28</u>	<u>102.57</u>
	S.D.	17.6	30.1	31.6	34.1	27.6	30.9	40.4
Total	Mean	<u>53.05</u>	<u>118.18</u>	<u>119.64</u>	<u>90.30</u>	<u>124.00</u>	<u>99.57</u>	
	S.D.	20.6	29.4	29.0	34.7	31.8	34.3	

A Scheffé analysis indicating significance of difference between total treatment mean scores appears in Table XV below. Included in this table is a graphic representation of the mean score values.

TABLE XV
BETA TIME SCHEFFÉ ANALYSIS

		<u>Treatment</u>	<u>Time(in seconds)</u>
<u>S indicates p<.05</u>		1. Rest	135
1 vs 2,3,4 - S		<u>Problem Solving</u>	125
1 vs 5,6 - S			115
2,3,4 vs 5,6 -		2. Mathematical	105
		3. Conceptualization	95
		4. Cumulative Number adding	85
			75
			65
		<u>Stress</u>	55
			45
		5. Color	
		6. Syringe	

The two dimensional repeated measures analysis for data recorded on the beta clock is presented in Table XVI on page 41. The Within Subjects F statistic of 70.47 indicates significance at the .05 level with respect to variability among the means of the six treatments. This further supports the hypothesis, with relation to beta time, that: "Brain wave patterns would be different, depending whether the subjects were resting, solving problems, or under stress." A simple ANOVA comparing high and low groups for each treatment condition resulted in no significant differences.

TABLE XVI
BETA TIME REPEATED MEASURES ANALYSIS

Source	DF	SS	MS	F	
Among Subjects					
B	1	952.22	952.22	.32	
Subjects(s)	48	141539.81	2948.75		
Within Subjects					
A	5	179344.50	35868.90	70.47	p<.05
AB	5	5837.09	1167.42	2.29	
AS	240	122158.56	508.99		
Total	299	449832.19			

The beta count mean scores and their associated standard deviations for the six treatments appear in Table XVII below.

TABLE XVII
BETA COUNT MEAN SCORES

		<u>Rest- ing</u>	<u>Math Prob</u>	<u>Con- cep- tual Prob</u>	<u>Cum num Prob</u>	<u>Color Stress</u>	<u>Syringe Stress</u>	<u>Total</u>
High	<u>Mean</u>	<u>365.20</u>	<u>430.04</u>	<u>449.56</u>	<u>427.40</u>	<u>418.20</u>	<u>398.16</u>	<u>414.75</u>
	<u>S.D.</u>	<u>84.4</u>	<u>66.5</u>	<u>61.8</u>	<u>93.4</u>	<u>98.1</u>	<u>99.9</u>	<u>89.8</u>
Low	<u>Mean</u>	<u>325.60</u>	<u>420.16</u>	<u>412.52</u>	<u>427.28</u>	<u>360.72</u>	<u>427.08</u>	<u>395.56</u>
	<u>S.D.</u>	<u>87.4</u>	<u>82.5</u>	<u>79.3</u>	<u>78.7</u>	<u>94.2</u>	<u>80.4</u>	<u>92.7</u>
Total	<u>Mean</u>	<u>345.40</u>	<u>425.10</u>	<u>431.04</u>	<u>427.34</u>	<u>389.44</u>	<u>412.62</u>	
	<u>S.D.</u>	<u>89.1</u>	<u>75.9</u>	<u>74.2</u>	<u>87.3</u>	<u>101.4</u>	<u>92.8</u>	

A Scheffe analysis indicating significance of difference between total treatment mean scores appears in Table XVIII on page 42. Included in this table is a graphic representation of the mean score values.

TABLE XIX
BETA COUNT REPEATED MEASURES ANALYSIS

Source	DF	SS	MS	F	
Among Subjects					
B	1	27629.00	27629.00	2.48	
Subjects(s)	48	534819.50	11142.07		
Within Subjects					
A	5	271668.00	54333.60	8.08	$p < .05$
AB	5	62038.50	12407.70	1.84	
AS	240	1614501.50	6727.09		
Total	299	2510656.50			

DATA RELATED TO SUB-LEVEL BRAIN WAVE MEASUREMENTS

The equipment was wired in such a way that, when none of the three brain waves produced by the subject were at or above the 10uv level, a fourth clock and separate counter tabulated the duration and extent of this state. The statistical analysis of this data is presented for completeness in reporting; however, conclusions from the analyses of these findings should be cautiously considered until such time as further research fully indicates their significance.

The sub-level time mean scores and their associated standard deviations for the six treatments are presented in Table XX on page 44.

TABLE XX
SUB-LEVEL TIME MEAN SCORES

		<u>Rest- ing</u>	<u>Math Prob</u>	<u>Con- cep- tual Prob</u>	<u>Cum- num Prob</u>	<u>Color Stress</u>	<u>Syringe Stress</u>	<u>Total</u>
High	<u>Mean</u>	<u>12.21</u>	<u>22.43</u>	<u>17.13</u>	<u>29.81</u>	<u>24.42</u>	<u>34.12</u>	<u>25.36</u>
	<u>S.D.</u>	<u>12.1</u>	<u>14.7</u>	<u>9.4</u>	<u>20.6</u>	<u>19.2</u>	<u>23.4</u>	<u>18.8</u>
Low	<u>Mean</u>	<u>26.45</u>	<u>22.35</u>	<u>18.63</u>	<u>34.24</u>	<u>16.64</u>	<u>30.03</u>	<u>24.75</u>
	<u>S.D.</u>	<u>30.5</u>	<u>17.1</u>	<u>15.9</u>	<u>27.3</u>	<u>17.1</u>	<u>24.6</u>	<u>23.7</u>
Total	<u>Mean</u>	<u>19.33</u>	<u>22.42</u>	<u>17.98</u>	<u>32.03</u>	<u>20.53</u>	<u>32.07</u>	
	<u>S.D.</u>	<u>24.5</u>	<u>16.1</u>	<u>13.2</u>	<u>24.5</u>	<u>18.7</u>	<u>24.4</u>	

A Scheffe' analysis indicating significance of difference between total treatment mean scores appears in Table XXI below. Included in this table is a graphic representation of the mean score values.

TABLE XXI
SUB-LEVEL TIME SCHEFFE' ANALYSIS

	<u>Treatment</u>	<u>Time(in seconds)</u>
	1. Rest	34
	<u>Problem Solving</u>	32
	2. Mathematical	30
	3. Conceptualization	28
	4. Cumulative Number Adding	26
	<u>Stress</u>	24
	5. Color	22
	6. Syringe	20

<u>S indicates p < .05</u>						
1 vs 2,3,4	-					
1 vs 5,6	-					
2,3,4 vs 5,6	-					
		<u>6</u>				
		<u>5</u>	<u>S</u>			
		<u>4</u>	<u>S</u>			
	<u>3</u>	<u>S</u>	<u>S</u>			
	<u>2</u>	<u>S</u>	<u>S</u>			
<u>1</u>	<u>S</u>	<u>S</u>				

Treatment	Time (in seconds)
1	34
2	32
3	30
4	28
5	26
6	24

The two dimensional repeated measures analysis for data recorded on the sub-level clock is presented in Table XXII below. The Within Subjects F statistic of 8.03 indicates significance at the .05 level with respect to variability among the means of the six treatments. This may further support the hypothesis, with relation to sub-level time, that: "Brain wave patterns would be different, depending whether the subjects were resting, solving problems, or under stress."

A simple ANCOVA comparing high and low groups for each treatment condition resulted in a significant F statistic for the resting treatment of 4.5 which is significant at the .05 level, and is shown in Appendix C. A simple ANOVA comparing high and low groups for each of the other five treatment conditions resulted in no significant differences.

TABLE XXII
SUB-LEVEL TIME REPEATED MEASURES ANALYSIS

Source	DF	SS	MS	F	
Among Subjects					
B	1	145.40	145.40	.11	
Subjects(s)	48	62060.00	1292.92		
Within Subjects					
A	5	10110.87	2022.17	8.03	p < .05
AB	5	3637.75	727.55	2.89	
AS	240	60437.11	251.82		
Total	299	136391.14			

The sub-level count mean scores and their associated standard deviations for the six treatments are in Table XXIII on page 46.

TABLE XXIII
SUB-LEVEL COUNT MEAN SCORES

		<u>Rest- ing</u>	<u>Math Prob</u>	<u>Con- cep- tual Prob</u>	<u>Cum- num Prob</u>	<u>Color Stress</u>	<u>Syringe Stress</u>	<u>Total</u>
High	<u>Mean</u>	83.48	210.44	133.40	207.60	214.08	246.96	190.99
	<u>S.D.</u>	51.8	89.0	62.2	75.2	97.2	129.3	102.2
Low	<u>Mean</u>	132.32	206.48	174.56	220.00	165.48	219.60	186.41
	<u>S.D.</u>	91.3	93.7	82.3	106.1	96.6	117.3	98.9
Total	<u>Mean</u>	107.90	208.46	176.38	213.80	189.78	233.28	
	<u>S.D.</u>	79.0	92.3	75.8	93.1	101.0	112.3	

A Scheffé analysis indicating significance of difference between total treatment mean scores appears in Table XXIV below. Included in this table is a graphic representation of the mean score values.

TABLE XXIV
SUB-LEVEL COUNT SCHEFFE ANALYSIS

	<u>Treatment</u>	<u>Relay Closures</u>
		245
<u>S indicates p < .05</u>	1. Rest	230
		215
		200
		185
		170
		155
	6	140
	5	125
	4	110
	3	
	2	
1	S	1
	S	2
	S	3
	S	4
	S	5
	S	6
	5. Color	
	6. Syringe	

The two dimensional repeated measures analysis for data recorded on the sub-level counter is shown in Table XXV below. The Within Subjects F statistic of 19.16 indicates significance at the .05 level with respect to variability among the means of the six treatments. This may further support the hypothesis, with relation to sub-level count, that: "Brain wave patterns would be different, depending whether the subjects were resting, solving problems, or under stress."

A simple ANOVA comparing high and low groups for each treatment condition resulted in a significant F statistic for the resting treatment of 5.2 which is significant at the .05 level, and is shown in Appendix C. A simple ANOVA comparing high and low groups for each of the other five treatment conditions resulted in no significant differences.

TABLE XXV
SUB-LEVEL COUNT REPEATED MEASURES ANALYSIS

Source	DF	SS	MS	F	
Among Subjects					
B	1	1577.87	1577.87	.06	
Subjects(s)	48	1254193.87	26129.04		
Within Subjects					
A	5	481606.37	96321.27	19.16	p<.05
AB	5	70215.37	14043.07	2.79	
AS	240	1206779.62	5028.25		
Total	299	3014373.12			

SUMMARY OF FINDINGS

The two dimensional repeated measures analysis of data recorded

for all treatment conditions indicated significance at the .05 level with respect to variability among the means of the six treatments. This supports the hypothesis, with relation to theta-alpha-beta time and count, that: "Brain wave patterns would be different, depending whether the subjects were resting, solving problems, or under stress."

The simple ANOVA analyses comparing high and low groups for each treatment condition involved forty-eight calculations. Four of the eight calculations involved in the resting treatment indicated significance at the .05 level. These four were the time and count analyses for alpha and sub-level readings. Of the remaining forty ANOVA calculations only the one dealing with beta count during the color stress treatment was significant ($p .05$). Thus, of forty-eight simple ANOVA analyses only five were significant at the .05 level. Since only 10.4% of the calculations are significant, a figure closely approaching chance, it is not possible to conclude that: "High and low grade point average students would have differing brain wave patterns."

CHAPTER V

SUMMARY AND SUGGESTIONS FOR FUTURE RESEARCH

SUMMARY OF STUDY

Hypotheses and Subjects. This study investigated the hypotheses that (1) brain wave patterns would significantly differ depending on whether the subjects were resting, solving problems, or under stress and that (2) high and low grade point average students would have differing brain wave patterns. The subjects were senior midshipmen at the United States Naval Academy. The high group was comprised of those whose cumulative grade point average was between 3.50 and 4.00; the low group was comprised of those whose cumulative grade point average was between 2.00 and 2.25.

Experimental Treatment and Instrumentation. The study involved the application of six different treatments over a seventeen minute total testing time. Brain wave measurements were recorded as the subjects were: (1) resting, (2) working a mathematics problem, (3) working a conceptualization problem, (4) doing cumulative number adding, (5) reacting to stress introduced into a reading exercise, and (6) reacting to stress induced by preparing to have blood drawn from their arm. An EEG was used to detect brain waves in the dependent variable. The amplified brain wave signal was then simultaneously separated into its theta-alpha-beta brain wave components. The amount of time spent in each brain wave state above a predetermined level during each treatment was recorded, as well as the number of times the brain wave signal went

above and below the prescribed threshold.

Statistical Analysis. Since six different treatments were applied, a two dimensional repeated measures design was employed in recognition of the effect each treatment might have on those that followed. This approach allowed for the analysis of the significance of the difference between treatment means in light of the interrelationship between treatment applications.

Because the assumption of homogeneity of equicovariance was not supported, a simple analysis of variance was calculated comparing means among subjects for each treatment.

FINDINGS

With respect to the fifty students tested, this study has found that there are significant differences in brain wave patterns depending whether subjects are resting, solving problems, or under stress. This result confirms findings by others that techniques exist for measuring brain wave activity which are capable of differentiating between some behaviors (treatments).

This project also attempted to determine whether significant differences exist between high and low grade point average students with respect to the production of brain waves during resting, problem solving, and stress treatments. Only five (10.4%) of the forty-eight ANOVA comparisons made to determine whether differences existed were significant at the .05 level; this result could be explained to occur by chance. The use of a stratified random sample as well as the

possible uniqueness of the subjects mitigates against applying a liberal interpretation to the significance of the data analyzed in this research.

CONCLUSIONS AND IMPLICATIONS

The first hypothesis of this study was that differing treatments (resting, solving problems, or under stress) would produce significantly different brain waves for all subjects. Within the assumptions and limitations listed in Chapter I, this hypothesis was supported with all statistical evaluations being significant at the .05 level.

The utility of establishing that differing treatments produce significantly different brain waves may well be that a method of automatically detecting some behavior (i.e., treatment) changes can be developed. An extension of this concept is the possibility that student shifts from problem solving to resting may be detected in such a way as to alert the student that, in fact, he is no longer paying attention to his studies.

Another implication of this detection capability is that future researchers may be able to more accurately determine the attention given by subjects to various tasks they are performing as part of a study.

The second hypothesis was that identical treatments applied to students who had high and low grade point averages would result in the production of statistically significant differences in their brain wave

patterns. This hypothesis is not supported by the statistical findings because only 10.4% of the evaluations were found to be significant and this could have occurred by chance. However, it can not be concluded from the results of this study that there are not differences between high and low. This aspect of the study may have been influenced by the fact that the subjects generally fell within the top 30% of their high school graduating class. Thus, although high and low groups were used, even the bottom group could be much higher in its academic potential than the rest of the population.

The study has provided further evidence of the capability that exists to measure brain waves in a way which will permit comparisons between groups. Before results can be operationally relied upon it will be necessary to conduct further research with more heterogeneous groups. In addition, it will be necessary to increase sample size so that results can be related to groups other than the one studied.

SUGGESTIONS FOR FUTURE RESEARCH

The following questions generated by the findings of this study deserve further research effort:

- (1) Do the results of this study hold up for other groups?
- (2) Does a significant difference in brain wave patterns exist between high and low academic achievers with relation to the general population?
- (3) Does the cost of measuring brain wave differences justify the expense and provide more useful information than is already available with paper and pencil tests?

(4) Is there a relationship between theta-alpha-beta brain waves and scores on psychological tests?

(5) Is there a difference in brain wave patterns between creative and non-creative persons?

(6) Do parents and their children show similar brain wave patterns within the same type of treatment situations?

(7) Does the very act of brain wave measurement have more or less effect on the results than the act of a person taking a paper and pencil test?

APPENDIX A

DATA COLLECTION SHEET

ERIC
Full Text Provided by ERIC

3 minutes conceptual problem

	<u>Time</u>	<u>Count</u>
theta	Test 29	Test 30
alpha	Test 31	Test 32
beta	Test 33	Test 34
sub-level	Test 35	Test 36
	(Treatment #3)	

3 minute cumulative number adding

	<u>Time</u>	<u>Count</u>
theta	Test 37	Test 38
alpha	Test 39	Test 40
beta	Test 41	Test 42
sub-level	Test 43	Test 44
	(Treatment #4)	

1 minute color stress test(*)

	<u>Time</u>	<u>Count</u>
theta	Test 45	Test 46
alpha	Test 47	Test 48
beta	Test 49	Test 50
sub-level	Test 51	Test 52
	(Treatment #5)	

1 minute syringe stress test(*)

	<u>Time</u>	<u>Count</u>
theta	Test 53	Test 54
alpha	Test 55	Test 56
beta	Test 57	Test 58
sub-level	Test 59	Test 60
	(Treatment #6)	

Total time under stress(5&6)

	<u>Time</u>	<u>Count</u>
theta	Test 61	Test 62
alpha	Test 63	Test 64
beta	Test 65	Test 66
sub-level	Test 67	Test 68

Total problem solving time(2&3&4)

	<u>Time</u>	<u>Count</u>
theta	Test 69	Test 70
alpha	Test 71	Test 72
beta	Test 73	Test 74
sub-level	Test 75	Test 76

An * indicates that these figures were multiplied by a factor of three when the analysis for repeated measures design was done so that all data would be in 3 minute increments.

All measurements in theta-alpha-beta were at the 10 microvolt level with sub-level times and counts indicating the amounts of these factors when none of the three states were above the 10 microvolt level.

All measurements were taken between O1 and T3 with a ground wire at the middle of the forehead. (G1 placed at O1, and G2 at T3). These locations are in accordance with the International Electrode placement system.

APPENDIX B

RAW SCORES FOR TEST NOS. 1 THROUGH 76

APPENDIX B

RAW SCORES FOR TEST NOS. 1 THROUGH 76

Table		Page
B1	Test Nos. 1 - 6	59
B2	Test Nos. 7 - 12	60
B3	Test Nos. 13 - 18	61
B4	Test Nos. 19 - 24	62
B5	Test Nos. 25 - 30	63
B6	Test Nos. 31 - 36	64
B7	Test Nos. 37 - 42	65
B8	Test Nos. 43 - 48	66
B9	Test Nos. 49 - 54	67
B10	Test Nos. 55 - 60	68
B11	Test Nos. 61 - 66	69
B12	Test Nos. 67 - 72	70
B13	Test Nos. 73 - 76	71

The sequence of subject data presentation is determined by the individual's cumulative grade point average. The first score is that of the man with the highest cumulative grade point average (QPR) and the next twenty-four scores are in descending order of QPR for the rest of the high group. The twenty-sixth score is that individual with the highest QPR in the low group and the fiftieth score belongs to the man with the lowest QPR in the low group.

T#1	T#2	T#3	T#4	T#5	T#6
3.93		101			
3.92		102			
3.92		103			
3.91		104			
3.9		105			
3.90		106			
3.89		107			
3.88		108			
3.87		109			
3.86		110			
3.85		111			
3.84		112			
3.83		113			
3.82		114			
3.81		115			
3.80		116			
3.79		117			
3.78		118			
3.77		119			
3.76		120			
3.75		121			
3.74		122			
3.73		123			
3.72		124			
3.71		125			
3.70		126			
3.69		127			
3.68		128			
3.67		129			
3.66		130			
3.65		131			
3.64		132			
3.63		133			
3.62		134			
3.61		135			
3.60		136			
3.59		137			
3.58		138			
3.57		139			
3.56		140			
3.55		141			
3.54		142			
3.53		143			
3.52		144			
3.51		145			
3.50		146			
3.49		147			
3.48		148			
3.47		149			
3.46		150			
3.45		151			
3.44		152			
3.43		153			
3.42		154			
3.41		155			
3.40		156			
3.39		157			
3.38		158			
3.37		159			
3.36		160			
3.35		161			
3.34		162			
3.33		163			
3.32		164			
3.31		165			
3.30		166			
3.29		167			
3.28		168			
3.27		169			
3.26		170			
3.25		171			
3.24		172			
3.23		173			
3.22		174			
3.21		175			
3.20		176			
3.19		177			
3.18		178			
3.17		179			
3.16		180			
3.15		181			
3.14		182			
3.13		183			
3.12		184			
3.11		185			
3.10		186			
3.09		187			
3.08		188			
3.07		189			
3.06		190			
3.05		191			

T#13	T#14	T#15	T#16	T#17	T#18
105.32	171	171.00	171	171.00	171
75.73	171	171.00	171	171.00	171
132.11	171	171.00	171	171.00	171
170.2	201	171.00	171	171.00	171
21.03	201	171.00	171	171.00	171
172.35	201	171.00	171	171.00	171
145.01	171	171.00	171	171.00	171
170.37	201	171.00	171	171.00	171
32.29	171	171.00	171	171.00	171
31.25	173	171.00	171	171.00	171
120.75	201	171.00	171	171.00	171
02.02	215	171.00	171	171.00	171
94.41	140	171.00	171	171.00	171
147.37	170	171.00	171	171.00	171
110.03	207	171.00	171	171.00	171
01.70	215	171.00	171	171.00	171
07.53	214	171.00	171	171.00	171
04.00	157	171.00	171	171.00	171
135.21	230	171.00	171	171.00	171
120.49	273	171.00	171	171.00	171
65.96	170	171.00	171	171.00	171
159.65	180	171.00	171	171.00	171
114.45	201	171.00	171	171.00	171
97.70	201	171.00	171	171.00	171
111.33	230	171.00	171	171.00	171
109.77	202	171.00	171	171.00	171
117.42	200	171.00	171	171.00	171
59.36	170	171.00	171	171.00	171
25.31	201	171.00	171	171.00	171
110.60	230	171.00	171	171.00	171
103.23	192	171.00	171	171.00	171
01.65	207	171.00	171	171.00	171
21.39	215	171.00	171	171.00	171
01.96	150	171.00	171	171.00	171
100.90	241	171.00	171	171.00	171
73.21	177	171.00	171	171.00	171
3.23	13	171.00	171	171.00	171
23.26	76	171.00	171	171.00	171
142.61	171	171.00	171	171.00	171
110.37	230	171.00	171	171.00	171
145.37	215	171.00	171	171.00	171
60.34	171	171.00	171	171.00	171
93.16	215	171.00	171	171.00	171
10.01	37	171.00	171	171.00	171
05.10	225	171.00	171	171.00	171
97.02	225	171.00	171	171.00	171
105.57	221	171.00	171	171.00	171
114.71	219	171.00	171	171.00	171
133.64	245	171.00	171	171.00	171
13.07	40	171.00	171	171.00	171

4

T#25	T#26	T#27	T#28	T#29	T#30
117.71	351	37.71	17	70.00	17
131.1	337	35.17	17	71.71	17
25.7	411	35.00	17	71.00	17
127.93	355	17.11	13	71.00	17
32.40	432	17.11	13	71.00	17
37.94	431	17.11	13	71.00	17
159.95	211	17.11	13	71.00	17
26.27	412	17.11	13	71.00	17
22.17	375	33.37	17	71.00	17
117.32	422	13.00	17	71.00	17
133.37	410	14.00	17	71.00	17
99.17	313	21.00	17	71.00	17
145.10	355	4.11	17	71.00	17
120.74	451	11.02	17	71.00	17
141.73	312	9.71	137	71.00	17
137.11	451	11.70	137	71.00	17
1.00	410	40.01	210	71.00	17
137.00	411	10.25	137	71.00	17
149.07	355	4.00	110	71.00	17
97.57	410	0.62	320	71.00	17
120.94	407	23.02	170	71.00	17
14.01	359	0.00	17	71.00	17
110.04	332	20.20	210	71.00	17
147.07	351	10.32	137	71.00	17
00.30	410	04.25	190	71.00	17
105.62	275	0.32	94	71.00	17
122.07	475	11.39	271	71.00	17
135.01	459	9.21	137	71.00	17
135.22	170	1.00	27	71.00	17
140.11	371	0.00	123	71.00	17
100.93	310	20.17	256	71.00	17
115.66	402	27.15	201	71.00	17
04.40	310	49.40	322	71.00	17
120.33	440	16.11	133	71.00	17
73.53	410	04.40	321	71.00	17
131.31	451	21.17	271	71.00	17
100.17	502	36.62	357	71.00	17
111.04	495	32.91	300	71.00	17
125.04	462	10.00	155	71.00	17
03.40	404	21.00	237	71.00	17
00.95	401	04.01	357	71.00	17
100.53	274	3.12	57	71.00	17
117.75	425	20.72	233	71.00	17
145.46	355	0.22	117	71.00	17
140.23	372	13.27	133	71.00	17
144.70	453	6.01	102	71.00	17
140.32	344	6.41	110	71.00	17
92.40	514	35.22	311	71.00	17
133.54	453	10.95	133	71.00	17

T#31	T#32	T#33	T#34	T#35	T#36
131.77	311	131.77	311	131.77	311
117.00	317	117.00	317	117.00	317
131.97	315	131.97	315	131.97	315
124.76	317	124.76	317	124.76	317
119.19	331	119.19	331	119.19	331
123.73	311	123.73	311	123.73	311
137.13	317	137.13	317	137.13	317
115.13	210	115.13	210	115.13	210
111.11	317	111.11	317	111.11	317
121.52	331	121.52	331	121.52	331
140.25	210	140.25	210	140.25	210
111.13	337	111.13	337	111.13	337
127.03	317	127.03	317	127.03	317
141.13	210	141.13	210	141.13	210
119.13	320	119.13	320	119.13	320
127.07	310	127.07	310	127.07	310
123.91	312	123.91	312	123.91	312
115.05	210	115.05	210	115.05	210
131.25	311	131.25	311	131.25	311
137.03	247	137.03	247	137.03	247
117.33	337	117.33	337	117.33	337
124.22	314	124.22	314	124.22	314
131.14	319	131.14	319	131.14	319
138.52	301	138.52	301	138.52	301
119.00	310	119.00	310	119.00	310
123.14	312	123.14	312	123.14	312
115.11	214	115.11	214	115.11	214
130.97	290	130.97	290	130.97	290
147.33	253	147.33	253	147.33	253
141.05	319	141.05	319	141.05	319
144.31	257	144.31	257	144.31	257
142.42	275	142.42	275	142.42	275
119.13	322	119.13	322	119.13	322
101.10	337	101.10	337	101.10	337
127.01	333	127.01	333	127.01	333
122.40	342	122.40	342	122.40	342
131.05	310	131.05	310	131.05	310
97.09	323	97.09	323	97.09	323
133.05	317	133.05	317	133.05	317
131.24	317	131.24	317	131.24	317
131.04	315	131.04	315	131.04	315
93.57	330	93.57	330	93.57	330
130.39	230	130.39	230	130.39	230
122.14	318	122.14	318	122.14	318
133.00	305	133.00	305	133.00	305
70.05	202	70.05	202	70.05	202
109.71	344	109.71	344	109.71	344
143.11	232	143.11	232	143.11	232
123.31	333	123.31	333	123.31	333
107.37	332	107.37	332	107.37	332
111.11	311	111.11	311	111.11	311
131.11	311	131.11	311	131.11	311
113.11	311	113.11	311	113.11	311
115.11	311	115.11	311	115.11	311
117.11	311	117.11	311	117.11	311
119.11	311	119.11	311	119.11	311
121.11	311	121.11	311	121.11	311
123.11	311	123.11	311	123.11	311
125.11	311	125.11	311	125.11	311
127.11	311	127.11	311	127.11	311
129.11	311	129.11	311	129.11	311
131.11	311	131.11	311	131.11	311
133.11	311	133.11	311	133.11	311
135.11	311	135.11	311	135.11	311
137.11	311	137.11	311	137.11	311
139.11	311	139.11	311	139.11	311
141.11	311	141.11	311	141.11	311
143.11	311	143.11	311	143.11	311
145.11	311	145.11	311	145.11	311
147.11	311	147.11	311	147.11	311
149.11	311	149.11	311	149.11	311
151.11	311	151.11	311	151.11	311
153.11	311	153.11	311	153.11	311
155.11	311	155.11	311	155.11	311
157.11	311	157.11	311	157.11	311
159.11	311	159.11	311	159.11	311
161.11	311	161.11	311	161.11	311
163.11	311	163.11	311	163.11	311
165.11	311	165.11	311	165.11	311
167.11	311	167.11	311	167.11	311
169.11	311	169.11	311	169.11	311
171.11	311	171.11	311	171.11	311
173.11	311	173.11	311	173.11	311
175.11	311	175.11	311	175.11	311
177.11	311	177.11	311	177.11	311
179.11	311	179.11	311	179.11	311
181.11	311	181.11	311	181.11	311
183.11	311	183.11	311	183.11	311
185.11	311	185.11	311	185.11	311
187.11	311	187.11	311	187.11	311
189.11	311	189.11	311	189.11	311
191.11	311	191.11	311	191.11	311
193.11	311	193.11	311	193.11	311
195.11	311	195.11	311	195.11	311
197.11	311	197.11	311	197.11	311
199.11	311	199.11	311	199.11	311
201.11	311	201.11	311	201.11	311
203.11	311	203.11	311	203.11	311
205.11	311	205.11	311	205.11	311
207.11	311	207.11	311	207.11	311
209.11	311	209.11	311	209.11	311
211.11	311	211.11	311	211.11	311
213.11	311	213.11	311	213.11	311
215.11	311	215.11	311	215.11	311
217.11	311	217.11	311	217.11	311
219.11	311	219.11	311	219.11	311
221.11	311	221.11	311	221.11	311
223.11	311	223.11	311	223.11	311
225.11	311	225.11	311	225.11	311
227.11	311	227.11	311	227.11	311
229.11	311	229.11	311	229.11	311
231.11	311	231.11	311	231.11	311
233.11	311	233.11	311	233.11	311
235.11	311	235.11	311	235.11	311
237.11	311	237.11	311	237.11	311
239.11	311	239.11	311	239.11	311
241.11	311	241.11	311	241.11	311
243.11	311	243.11	311	243.11	311
245.11	311	245.11	311	245.11	311
247.11	311	247.11	311	247.11	311
249.11	311	249.11	311	249.11	311
251.11	311	251.11	311	251.11	311
253.11	311	253.11	311	253.11	311
255.11	311	255.11	311	255.11	311
257.11	311	257.11	311	257.11	311
259.11	311	259.11	311	259.11	311
261.11	311	261.11	311	261.11	311
263.11	311	263.11	311	263.11	311
265.11	311	265.11	311	265.11	311
267.11	311	267.11	311	267.11	311
269.11	311	269.11	311	269.11	311
271.11	311	271.11	311	271.11	311
273.11	311	273.11	311	273.11	311
275.11	311	275.11	311	275.11	311
277.11	311	277.11	311	277.11	311
279.11	311	279.11	311	279.11	311
281.11	311	281.11	311	281.11	311
283.11	311	283.11	311	283.11	311
285.11	311	285.11	311	285.11	311
287.11	311	287.11	311	287.11	311
289.11	311	289.11	311	289.11	311
291.11	311	291.11	311	291.11	311
293.11	311	293.11	311	293.11	311
295.11	311	295.11	311	295.11	311
297.11	311	297.11	311	297.11	311
299.11	311	299.11	311	299.11	311
301.11	311	301.11	311	301.11	311
303.11	311	303.11	311	303.11	311
305.11	311	305.11	311	305.11	311
307.11	311	307.11	311	307.11	311
309.11	311	309.11	311	309.11	311
311.11	311	311.11	311	311.11	311

T#37	T#38	T#39	T#40	T#41	T#42
31.59	11	117.15	11	117.07	11
11.51	7	150.5	21	117.51	11
11.51	215	150.55	220	117.55	11
52.45	155	117.57	35	118.15	11
21.55	27	117.15	12	118.7	11
54.50	175	117.5	175	118.71	11
55.71	17	121.57	215	118.55	11
55.52	110	117.7	215	118.5	11
21.57	22	17.51	217	118.5	11
55.52	174	15.57	21	118.5	11
21.55	155	111.51	21	118.55	11
21.52	221	150.5	111	118.55	11
22.47	225	151.55	11	118.25	11
22.16	20	155.5	355	118.54	11
57.97	155	121.55	151	57.5	11
58.5	112	151.57	212	118.55	11
58.75	152	117.55	215	111.55	11
112.11	232	165.77	155	125.1	11
59.15	207	151.77	267	157.54	11
21.46	37	97.51	205	59.58	11
31.2	111	155.77	355	137.55	11
59.21	275	129.39	315	117.52	11
54.50	171	152.5	149	55.51	11
54.55	124	110.55	305	107.22	11
117.46	205	175.59	52	57.79	11
65.13	195	157.57	305	179.51	11
42.34	156	115.47	305	27.75	11
73.60	195	134.57	217	11.75	11
127.55	242	167.42	155	154.95	11
52.5	214	149.25	275	157.55	11
72.90	263	126.55	315	24.57	11
51.12	155	104.77	351	20.5	11
51.01	157	119.95	25	111.52	11
41.05	136	125.23	271	5.21	11
23.53	75	53.51	255	51.22	11
15.15	62	52.76	315	72.24	11
33.26	114	105.60	257	49.21	11
57.23	151	116.22	339	170.65	11
17.59	224	155.50	175	155.51	11
51.16	153	112.11	255	65.11	11
34.92	79	75.42	357	48.42	11
52.25	156	141.17	275	155.34	11
57.55	124	107.71	317	165.55	11
45.77	151	120.57	319	134.66	11
15.14	57	52.92	250	53.61	11
35.50	139	105.44	264	53.30	11
44.54	142	97.79	315	71.95	11
11.92	270	171.54	59	107.72	11
11.77	45	79.46	357	63.52	11

T#61	T#62	T#63	T#64	T#65	T#66
10.00	101	10.00	101	10.00	101
11.41	101	10.00	101	10.00	101
10.00	101	10.00	101	10.00	101
34.57	101	31.50	115	31.50	115
21.24	101	10.00	115	10.00	115
30.00	101	10.00	121	10.00	121
30.20	122	21.10	101	21.10	101
11.40	101	30.00	101	30.00	101
10.10	101	30.00	101	30.00	101
30.20	120	31.00	101	31.00	101
41.00	120	30.00	101	30.00	101
30.00	110	71.20	101	70.00	101
40.37	102	21.00	120	21.00	101
20.00	101	10.00	101	10.00	101
10.00	101	30.00	101	30.00	101
30.00	101	11.10	211	10.00	101
20.00	101	30.00	207	21.00	101
47.00	120	70.24	207	10.20	101
39.07	111	10.70	210	10.07	101
10.00	101	30.00	101	30.00	101
20.00	101	10.00	101	10.00	101
30.00	101	20.00	101	10.00	101
10.10	101	30.00	101	30.00	101
41.30	121	20.00	110	20.00	101
40.00	127	30.00	101	30.00	101
30.72	100	12.27	101	11.50	101
30.00	110	70.00	201	20.00	101
47.94	120	39.01	110	70.01	101
30.70	130	27.00	101	21.11	101
30.00	140	20.10	120	100.10	101
39.10	114	77.40	220	20.00	101
27.97	101	12.00	210	12.00	101
24.40	101	04.00	210	02.00	101
39.07	122	07.00	170	00.00	101
12.40	101	40.01	101	03.10	101
29.14	100	19.00	101	00.01	101
20.00	101	00.10	210	00.01	101
10.00	101	00.00	200	00.00	101
40.11	141	04.00	101	04.10	101
40.94	131	19.00	210	00.00	101
20.00	101	00.00	200	00.00	101
30.00	101	101.04	170	04.00	101
30.00	101	70.00	210	00.00	101
30.00	101	90.70	101	100.00	101
30.00	101	70.00	220	00.00	101
51.00	127	00.10	101	00.00	101
30.37	127	22.10	101	00.00	101
17.04	122	31.00	101	10.00	101
22.00	101	07.00	231	00.00	101

T#67	T#68	T#69	T#70	T#71	T#72
122.42		122.42			
151.6		151.6			
257.67		257.67			
151.6		151.6			
217.64		217.64			
125.61		125.61			
151.7		151.7			
265.62		265.62			
111.52		111.52			
151.95		151.95			
195.75		195.75			
155.44		155.44			
225.22		225.22			
250.86		250.86			
112.55		112.55			
162.66		162.66			
156.52		156.52			
150.01		150.01			
259.79		259.79			
256.49		256.49			
100.57		100.57			
115.90		115.90			
266.02		266.02			
163.02		163.02			
151.61		151.61			
250.61		250.61			
216.09		216.09			
221.59		221.59			
244.62		244.62			
339.53		339.53			
235.11		235.11			
205.97		205.97			
146.43		146.43			
153.53		153.53			
152.83		152.83			
95.64		95.64			
109.86		109.86			
124.65		124.65			
139.49		139.49			
265.35		265.35			
197.65		197.65			
124.69		124.69			
246.45		246.45			
146.12		146.12			
166.19		166.19			
116.29		116.29			
177.23		177.23			
195.15		195.15			
259.68		259.68			
121.54		121.54			

APPENDIX C

ANOVA FOR TEST NOS. 1 THROUGH 76

APPENDIX C

ANOVA for Test Nos. 1 through 76

F significant @: .005 - 8.695 .01 - 7.201 .025 - 5.369 .05 - 4.052 .10 - 2.815 .25 - 1.356

Degrees of Freedom: Among Columns 1 Error(within) 48 Total 49 Grp 1-High Grp 2-Low

No	Title	Std. Dev.		Mean		Sum of Squares		Mean Squares		F	
		Grp 1	Grp 2	Grp 1	Grp 2	AC	EW	AC	EW		
1	Gr Pt Av (QPR)	.1	.1	3.7	2.2	30.1	.6	30.6	30.1	.0	2554.9
2	Apt-Verbal	75.4	48.0	634.3	566.5	57460.5	199676.0	257136.0	57460.5	4159.9	13.8
3	Apt-Math	47.4	67.4	697.6	633.3	51584.7	169721.0	221306.0	51584.7	3535.9	14.6
4	Ach-Eng Comp	72.7	61.0	611.1	556.5	37210.0	224808.0	262018.0	37210.0	4683.5	7.3
5	Ach-Math	58.0	54.3	727.2	620.0	143755.0	159489.0	303244.0	143755.0	3322.7	43.3
6	Rank in Class	96.4	78.2	650.0	508.1	251766.0	385470.0	637236.0	251766.0	8030.6	31.4
7	Recom Score	31.3	105.3	760.8	677.0	87780.5	301612.0	389392.0	87780.5	6283.6	14.0
8	Extra Cur Activ	104.5	150.6	479.8	506.6	8978.0	839810.0	848788.0	8978.0	17496.0	.5
9	Whole-Man-Mult	3919.0	5621.8	63258.0	5705.4	4824700.0	117406000.0	165651000.0	4824700.0	2445568.0	19.7
10	CWF 2	3.2	2.9	3.4	3.6	.2	470.3	470.5	.2	9.8	.0
11	Hay Fever	3.7	3.7	13.4	13.4	0.0	672.0	672.0	0.0	14.0	0.0
12	L or R Handed	3.7	3.2	13.4	13.8	2.0	600.0	602.0	2.0	12.5	.2
13	Rest-Theta-Time	29.5	40.6	103.6	87.5	3238.8	62951.0	66199.8	3238.8	1311.7	2.5
14	Rest-Theta-Count	35.2	67.6	211.6	185.5	8528.2	145258.0	153786.0	8528.2	3026.2	2.8
15	Rest-Alpha-Time	13.9	33.3	160.2	141.3	4454.0	32482.9	36936.9	4454.0	676.7	6.6
16	Rest-Alpha-Count	54.7	95.4	120.1	176.9	40334.8	307160.0	347544.0	40334.8	6399.2	6.3
17	Rest-Beta-Time	21.5	17.6	58.6	47.5	1520.8	19262.2	20783.0	1520.8	401.3	3.8
18	Rest-Beta-Count	84.4	87.4	365.2	325.6	19602.0	369342.0	388944.0	19602.0	7694.6	2.5
19	Rest-S/L-Time	12.1	30.5	12.2	26.5	2534.9	26885.8	29420.6	2534.9	560.1	4.5
20	Rest-S/L-Count	51.8	91.3	83.5	132.3	29816.8	275646.0	305462.0	29816.8	5742.6	5.2
21	Math-Theta-Time	21.8	20.4	56.0	57.9	44.2	22317.6	22361.8	44.2	464.9	.1
22	Math-Theta-Count	44.8	36.7	165.0	168.4	141.1	83733.8	83874.9	141.1	1744.5	.1
23	Math-Alpha-Time	17.6	20.3	121.5	120.8	5.5	18008.1	18013.5	5.5	375.2	.0
24	Math-Alpha-Count	28.7	30.1	300.6	303.3	89.8	43227.1	43316.8	89.8	900.6	.1

F significant @: .005 - 8.695 .01 - 7.201 .025 - 5.369 .05 - 4.052 .10 - 2.815 .25 - 1.356

Degrees of Freedom: Among Columns 1 Error(within) 48 Total 49 Grp 1-High Grp 2-Low

No	Title	Std. Dev.		Mean		Sum of Squares		Mean Squares		F	
		Grp 1	Grp 2	Grp 1	Grp 2	AC	EW	AC	EW		
25	Math-Beta-Time	27.9	30.1	117.3	119.0	36.9	42230.1	42267.0	36.9	879.8	.0
26	Math-Beta-Count	66.5	82.5	430.0	420.2	1220.1	280844.0	282064.0	1220.1	5850.9	.2
27	Math-S/L-Time	14.7	17.1	22.5	22.3	.2	12673.8	12674.1	.2	264.0	.0
28	Math-S/L-Count	89.0	93.7	210.4	205.5	196.0	417506.0	417702.0	196.0	8698.1	.0
29	Concep-Theta-Time	17.9	19.2	69.5	73.9	242.2	17208.1	17450.2	242.2	358.5	.7
30	Concep-Theta-Count	23.9	25.8	190.6	195.3	269.1	30918.8	31187.9	269.1	644.1	.4
31	Concep-Alpha-Time	12.1	19.4	127.2	124.4	101.2	13946.6	13147.8	101.2	271.8	.4
32	Concep-Alpha-Count	22.3	28.4	305.9	307.1	19.3	32579.2	32598.5	19.3	678.7	.0
33	Concep-Beta-Time	25.4	31.6	119.3	120.0	7.1	41125.8	41132.9	7.1	856.8	.0
34	Concep-Beta-Count	61.8	79.3	449.6	412.5	17149.5	252564.0	269714.0	17149.5	5261.8	3.3
35	Concep-S/L-Time	9.4	15.9	17.1	18.8	36.0	8500.1	8536.1	36.0	177.1	.2
36	Concep-S/L-Count	62.2	82.3	183.4	174.6	976.8	266146.0	267123.0	976.8	5544.7	.2
37	CumNum-Theta-Time	23.6	31.1	52.2	56.4	221.0	38117.4	38338.4	221.0	794.1	.3
38	CumNum-Theta-Count	47.6	62.2	153.1	156.4	134.5	153312.0	153446.0	134.5	3194.0	.0
39	CumNum-Alpha-Time	23.6	32.3	125.5	117.5	791.2	40102.5	40893.7	791.2	835.5	.9
40	CumNum-Alpha-Count	59.7	78.8	255.8	263.0	655.2	244051.0	244706.0	655.2	5084.4	.1
41	CumNum-Beta-Time	34.6	34.1	89.5	91.1	31.7	59096.3	59128.0	31.7	1231.2	.0
42	CumNum-Beta-Count	93.4	78.7	427.4	427.3	.3	373019.0	373019.0	.3	7771.2	.0
43	CumNum-S/L-Time	20.6	27.3	29.8	34.2	244.8	29286.1	29531.0	244.8	610.1	.4
44	CumNum-S/L-Count	75.2	106.1	207.6	220.0	1922.0	422804.0	424726.0	1922.0	8808.4	.2
45	Color-Theta-Time	6.9	8.6	18.4	21.8	137.8	3019.6	3157.4	137.8	62.9	2.2
46	Color-Theta-Count	13.5	13.1	55.2	59.3	204.0	8839.6	9043.6	204.0	184.2	1.1
47	Color-Alpha-Time	7.0	6.9	39.0	41.4	73.3	2406.8	2480.1	73.3	50.1	1.5
48	Color-Alpha-Count	10.1	14.3	101.8	101.5	1.3	7634.2	7635.5	1.3	159.0	.0
49	Color-Beta-Time	10.9	9.2	38.5	44.1	396.0	5107.2	5503.2	396.0	106.4	3.7
50	Color-Beta-Count	32.7	31.4	139.4	120.2	4588.8	51344.6	55933.4	4588.8	1069.7	4.3
51	Color-S/L-Time	6.4	5.7	8.1	5.5	84.2	1810.5	1894.7	84.2	37.7	2.2
52	Color-S/L-Count	32.4	32.2	71.4	55.2	3280.5	52235.1	55515.6	3280.5	1088.2	3.0
53	Syringe-Theta-Time	6.6	7.3	15.9	17.4	26.3	2436.9	2463.2	26.3	50.8	.5

F significant @: .005 - 8.695 .01 - 7.201 .025 - 5.369 .05 - 4.052 .10 - 2.815 .25 - 1.356

Degrees of Freedom: Among Columns 1 Error(within) 48 Total 49 Grp 1-High Grp 2-Low

No	Title	Std. Dev.		Mean		Sum of Squares			Mean Squares		
		Grp 1	Grp 2	Grp 1	Grp 2	AC	EW	T	AC	EW	F
54	Syringe-Theta-Count	16.9	15.5	48.2	50.6	72.0	3131.5	13203.5	72.0	273.6	.3
55	Syringe-Alpha-Time	7.0	8.3	37.7	37.9	.3	2958.0	2958.3	.3	61.6	.0
56	Syringe-Alpha-Count	1.0	13.8	93.9	96.5	87.1	7808.9	7896.0	87.1	162.7	.5
57	Syringe-Beta-Time	11.9	10.3	31.3	35.1	180.9	6224.6	6405.5	180.9	129.7	1.4
58	Syringe-Beta-Count	33.3	26.8	132.7	142.4	1161.6	45708.8	46870.4	1161.6	952.3	1.2
59	Syringe-S/L-Time	7.8	8.2	11.4	10.0	23.2	3206.4	3229.6	23.2	65.8	.3
60	Syringe-S/L-Count	43.1	29.1	82.3	73.2	1039.7	67639.4	68679.1	1039.7	1409.2	.7
61	Tot Str-Theta-Time	12.4	13.7	34.4	39.1	283.6	8586.3	8869.9	283.6	178.9	1.6
62	Tot Str-Theta-Count	27.9	24.5	103.4	109.8	518.4	34465.4	34983.8	518.4	718.0	.7
63	Tot Str-Alpha-Time	12.6	13.5	76.7	79.3	83.6	8508.3	8591.9	83.6	177.3	.5
64	Tot Str-Alpha-Count	17.2	17.6	195.7	198.0	67.3	15097.4	15164.7	67.3	314.5	.2
65	Tot Str-Beta-Time	20.9	17.3	69.8	79.2	1109.1	18334.6	19443.7	1109.1	382.0	2.9
66	Tot Str-Beta-Count	49.8	43.9	273.4	262.6	1468.8	110282.0	111751.0	1468.8	2297.5	.6
67	Tot Str-S/L-Time	12.7	11.9	19.5	15.6	195.6	7595.4	7791.0	195.6	158.2	1.2
68	Tot Str-S/L-Count	64.8	52.6	157.7	128.4	10745.8	174103.0	184849.0	10745.8	3627.2	3.0
69	Tot Prob-Theta-Time	53.5	60.9	177.6	188.1	1374.5	164299.0	165673.0	1374.5	3422.9	.4
70	Tot Prob-Theta-Count	99.8	105.5	508.7	520.0	1590.5	527187.0	528777.0	1590.5	10983.1	.1
71	Tot Prob-Alpha-Time	44.7	60.1	374.2	362.7	1644.4	140397.0	142041.0	1644.4	2924.9	.6
72	Tot Prob-Alpha-Count	82.0	93.6	862.2	873.4	1557.0	387270.0	388827.0	1557.0	8068.1	.2
73	Tot Prob-Beta-Time	77.3	78.7	326.1	330.1	206.6	304297.0	304504.0	206.6	6339.5	.0
74	Tot Prob-Beta-Count	142.3	183.2	1307.1	1221.3	92020.0	1344415.0	1436435.0	92020.0	28008.6	3.3
75	Tot Prob-S/L-Time	57.6	48.8	75.6	75.4	.3	142658.0	142658.0	.3	2972.0	.0
76	Tot Prob-S/L-Count	188.9	227.7	601.4	601.0	2.0	2188899.0	2188901.0	2.0	45602.1	.0

SELECTED BIBLIOGRAPHY

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BOOKS

- Brown, Clinton C. Methods in Psychophysiology. Baltimore: The Williams & Wilkins Company, 1967.
- Campbell, Donald T. and Stanley, Julian C. Handbook of Research on Teaching. Editor N. L. Gage. Chicago: Rand McNally, 1963.
- Cohn, Robert. Clinical Electroencephalography. New York: McGraw-Hill Book Company, Inc., 1949.
- Edwards, Allen L. Experimental Design in Psychological Research. New York: Holt, Rinehart and Winston, 1960.
- Ertl, J. P. "Evoked Potentials, Neural Efficiency, and IQ," in Biocybernetics of the Central Nervous System. Editor Lorne D. Proctor. Boston: Little, Brown and Company, 1969.
- Gage, Norman L. Handbook of Research on Teaching. Chicago: Rand McNally and Company, 1963.
- Glass, Gene V., and Stanley, Julian C. Statistical Methods in Education and Psychology. Englewood Cliffs: Prentice-Hall, Inc., 1970.
- Hill, Denis and Parr, Geoffrey. Electroencephalography. New York: The MacMillan Company, 1952.
- Knott, John R. "The Physiological Correlates of Intelligence," in NSSE Thirty-Ninth Yearbook, Part 1: Intelligence: Its Nature and Nurture. Bloomington: Public School Publishers, 1940.
- Lilly, J. C. "A Method of Recording the Moving Electrical Potential Gradient in the Brain: A 25-Channel Potential Field Recorder," in Proceedings Second Annual Joint IRE-AIEE Conference on Electronic Instrumentation in Nucleonics and Medicine. New York: IRE-AIEE, 1949.
- Lindsley, D. B. "Electroencephalography," in Personality and Behavior Disorders. Editor J. McV. Hunt. New York: Ronald Press, 1944.
- Luce, Gay Gaer. Biological Rhythms in Human and Animal Physiology. New York: Dover Publications, 1971.

- Milnarich, R. F., and Potts, F. A Manual for EEG Technicians. Boston: Little, Brown and Company, 1958.
- Nosal, Walter S. A Primer for Counseling the College Male. Dubuque: Wm. C. Brown Book Company, 1968.
- Pribram, K. H. Brain and Behaviour 2 - Perception and Action. Baltimore: Penguin Books Inc., 1969.
- Pribram, K. H. Brain and Behaviour 4 - Adaptation. Baltimore: Penguin Books Inc., 1969.
- Safe Use of Electricity in Hospitals 1971. Boston: National Fire Protection Association, 1971.
- Schwab, Robert S. Electroencephalography In Clinical Practice. Philadelphia: W. B. Saunders Company, 1951.
- Strauss, H., Ostow, M., and Greenstein, L. Diagnostic Electroencephalography. New York: Grune & Stratton, 1952.
- Walter, Carl W. Electric Hazards in Hospitals. Washington D. C.: National Academy of Sciences, 1970.
- Winer, B. J. Statistical Principles in Experimental Design. New York: McGraw-Hill Book Company, Inc., 1962.

ARTICLES

- Bennett, W. F. "Human Perception: a Network Theory Approach," Nature, 220 (December, 1968), 1148.
- Burch, N. R. "Automatic Analysis of the Electroencephalogram: A Review and Classification of Systems," Electroencephalography and Clinical Neurophysiology, 11 (November, 1959), 827-834.
- Cohn, Robert. "A Cycloscopic Study of the Human Electroencephalogram," Journal of General Physiology, 25 (March, 1942), 517-522.
- Darrow, C. W., and Hicks, R. "Interarea EEG Phase Relationships Following Sensory and Ideational Stimuli," Psychophysiology, 1 (April, 1965), 337-346.
- Ellingson, R. J. "Brain Waves and Problems in Psychology," Psychological Bulletin, 53 (January, 1956), 1-34.

- Ellingson, Robert J. "Relationship Between EEG and Test Intelligence: A Commentary," Psychological Bulletin, 65 (February, 1966), 96.
- Ertl, John P. "Fourier Analysis of Evoked Potentials and Human Intelligence," Nature, 230 (April, 1971), 526.
- Ertl, John P., and Schafer, Edward W. P. "Brain Response Correlates of Psychometric Intelligence," Nature, 223 (July, 1969), 422.
- Goodwin, C. W., and Stein, S. N. "A Brain Wave Correlator," Science, 108 (November, 1948), 507.
- Lang, Peter J. "The On-Line Computer in Behavior Therapy Research," American Psychologist, 24 (March, 1969), 236-239.
- MacKay, D. M., and McCulloch, W. S. "The Limiting Information Capacity of a Neuronal Link," Bulletin of Mathematical Biophysics, 14 (June, 1952), 127-135.
- Mundy-Castle, A. C. "Electrophysiological Correlates of Intelligence," Journal of Personality, 26 (March, 1958), 184-199.
- Oliver, Shirley. "Artifacts in EEG Recordings in Intensive Care Units." Spike and Wave, 18 (March, 1969), 1-18.
- Paskewitz, David A. "A Hybrid Circuit to Indicate the Presence of Alpha Activity." Accepted for publishing in Psychophysiology.
- Roy, E., Herrington, R. N., and Sutton, Samuel. "Effects of Visual Form on the Evoked Response," Science, 155 (March, 1967), 1439.
- Sonneman, H., and Kennard, M. A. "An Interphase Analyzer of the Electroencephalogram," Science, 105 (April, 1947), 437-438.
- Sutton, S., Braren, M., Zubin, J., and John, E. R. "Evoked Potential Correlates of Stimulus Uncertainty," Science, 150 (November, 1965), 1187-1188.
- Tracy, William. "Goodbye IQ, Hello EI (Ertl Index)," Phi Delta Kappan, 54 (October, 1972), 89-94.
- Vogel, William and Broverman, Donald M. "Relationship Between EEG and Test Intelligence: A Critical Review," Psychological Bulletin, 62 (August, 1964), 132-144.
- Vogel, William and Broverman, Donald M. "A Reply to 'Relationship Between EEG and Test Intelligence: A Commentary,'" Psychological Bulletin, 65 (February, 1966), 99.

REPORTS

Alpha and Beta Brain Waves. A report bibliography from the Defense Documentation Center, No. 052309, 14 Dec 1970.

Bibliography of Physiological Feedback. 250 author abstracted reports distributed by The Bio-Feedback Research Society, 1970.

Brain Waves. A report bibliography from the Defense Documentation Center, No. 052308, 14 Dec 1970.

Encephalography Research. A report bibliography from the Defense Documentation Center, No. 052310, 14 Dec 1970.